Intracavitary Brachytherapy in Cervical Carcinoma: The Role of F18-FDG-PET in Treatment Planning

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Abstract

Objective: concomitant chemoradiation with cisplatinum and intracavitary brachytherapy (BT) is the standard of care in patients with locally advanced cervix cancer. Treatment planning for BT provides for the use of three dimensional imaging, such as CT scan or MRI. Positron emission Tomography with [18F] FDG currently used in staging and restaging of this malignancy, is an imaging modality that can aid in image-guided radiation treatment planning. The purpose of our feasibility study was to compare two tumour volumes during BT planning, the CT-based and PET/CT-based clinical target volume (CTVs), in order to evaluate the value of functional imaging in BT planning and if it could be related to a CT standard data set. Moreover a correlation with some clinical data after a median follow up of 47 months is reported.

Methods: From June 2007 to May 2010, thirteen women with advanced cervical carcinoma were enrolled into the study. All the patients had a pretreatment PET/CT for staging. All BT fractions have been planned by CT scan and, in the first (BT1) and in the fourth fraction (BT4), FDG-PET/CT was also employed. Two volumes (CTVs) were defined: a CTVstandard, based on clinical information and on CT scan; and a CTVPET-influenced created with the additional information brought by PET scan.

Results: We compared the dimension of the two volumes and the intersection of CTVstandard and CTVPET-influenced at BT1 and BT4. A non-parametric sum rank test was used to determine the statistical significance for comparison of the two series of volumes (CTVstandard and CTVPET-influenced at BT1 and BT4). All patients completed the protocol, but out of 26 attempts of double CTV definition, only for 21 cases a comparison between CTVstandard and CTVPET-influenced was made. For two patients at the first BT fraction PET was negative. In the 21 valuable cases, considering both fractions together (BT1 and BT4), the difference between CTVstandard (25.8 ± 7.5 ml) and CTVPET-influenced (21.6 ± 9.5 ml) was statistically significant (p=0.01). In our small population the changes of CTVPET-influenced was unpredictable with residual tracer uptake areas often located far from the applicator and not consistent with clinical evaluation and or CT information.

Conclusions: Even if the results of the study are preliminary because of the limited number of patients, our data suggests that PET scan cannot be used to define target volume in BT plan as the only source of information. It could be necessary an integration preferably with MRI for much more individualized brachytherapy treatment.

Keywords: Brachytherapy; Cervical carcinoma; PET/CT treatment planning

Introduction

Concomitant chemo-radiation with cisplatinum and intracavitary brachytherapy (BT) is the standard of care in patients with locally advanced cervix cancer [1-4]. The knowledge of the real tumour size is an important prognostic factor for the outcome of the patient [5-7], so the modern BT needs 3D treatment planning as it allows to conform the dose distribution to the target volume and to minimize toxicity to normal tissues.

Historical dose prescription in BT is based on Manchester system that was designed to deliver a specific dose to a reference point (point A) [8], independently of three-dimensional spread of tumour volume. This point has no relationship with tumour position and real three-dimensional tumour extent [9,10]. Image-based BT treatment planning has been studied using computed tomography (CT) [11-13] or magnetic resonance imaging (MRI) [14].

MRI is considered the best imaging modality for tumour delineation in image-based intracavitary BT [15]; this superiority lies in its better contrast resolution that permits to distinguish tumour from normal uterine, vaginal and other surrounding tissues [16,17] and so, for its properties, is the best choice to define the reference volumes according to (GYN) GEC-ESTRO recommendations (2006) [18]. 18 Fluoro-deoxi-glucose Positron Emission Tomography (18F-FDG PET) is a functional imaging technique able to visualize the glucose consumption of tissue, that is one of the most represented metabolic pathways of viable neoplastic lesions. For this reason, PET and PET/CT scan have been studied in radiation treatment planning of different types of tumours [19-21].

In some previously published papers, 18F-FDG PET has been used...
for the volume definition of the primary cervical cancer [22] and also in BT plan [10,23-25], but one of the most important shortcoming was the lack of anatomical markers that can make difficult to distinguish physiological uptake of pelvic organs (i.e. ureters, bowel) from that of neoplastic lesions. In this context the use of hybrid PET/CT scanner, consisting of a PET scanner coupled with a CT scanner on line, could be of help in definition of BT planning in cervical cancer.

Considering these issues, the aim of our feasibility study was to compare the standard CT-based and PET/CT-based clinical target volume (CTV) in BT planning and the assessment of the added benefit of metabolic imaging in BT of cervical cancer.

Materials and Methods

Patient population

From June 2007 to May 2010 thirteen women with biopsy proven locally advanced squamous cervical carcinoma were enrolled into the study at the Radiation Oncology Department of San Gerardo Hospital in Monza. Patient characteristics are summarized in table 1. All the patients had whole body PET/CT for staging before treatment. Written informed consent was obtained from all patients.

Radiation therapy and chemotherapy protocol

All patients underwent external beam radiotherapy to the whole pelvis with a box technique (EBT-1.8 Gy/fraction to a total dose of 50.4 Gy over 6 weeks), with weekly concomitant cisplatin chemotherapy (40 mg/m²). High Dose Rate-BT was performed during the course of pelvic radiation therapy, in order to reduce the total treatment time, starting in the third week of EBT (5 Gy/fraction to 5-6 fractions). A complete vaginal and rectal examination of the clinical extension of the pelvic disease was performed in all the patients before the insertion of the standard Fletcher-Suit tandem. The PET/CT scans were performed and analyzed exclusively in order to produce a simulation of optimized BT plan; all the patients were actually treated under standard conditions.

18F-FDG PET/CT Scanning

Before starting PET/CT scan for BT planning, at the first and the fourth BT fraction (BT1 and BT4) a Fletcher–Suit tandem was positioned in order to simulate the organs position in BT treatment. The patient fastened for 6-8 hours before the scan and blood glucose (cut-off level 170 mg/dl) was determined immediately before the scan. Intravenous hydration and diuretic agent were administered to reduce the bladder activity. For the scan, a CT (120 kV, 80 mA, 3.75 slice thickness) covering the whole pelvis was performed first, then PET was performed acquiring two bed positions (5 minutes/bed) covering the whole pelvis. PET images were reconstructed with iterative algorithm and scatter correction.

PET based (GTVpet) and CT based (GTVct) volume definition

The transaxial, coronal and sagittal PET/CT images were displayed on an Advantage Windows Workstation (GE Healthcare, Milwaukee, WI-US) with predefined window levels and colour, according internal display protocol for volume definition on PET images. The contouring of the metabolic volume was visually defined on transaxial PET images by the nuclear medicine physician. A GTVpet (according to ICRU 83-2010) was obtained from each FDG-PET/CT study acquired before BT fractions for the BT1 and for the BT4. The PET contouring was automatically transferred to the coregistered CT images. These PET/CT fusion images were then sent to Oncentra Radiation treatment Planning system (Oncentra Masterplan, Nucletron, Veenendaal, The Netherlands), by which the radiation oncologist defined the target volume on the CT images (GTVct) and, in the same way, critical organs (bladder and rectum).

Clinical Target Volume (CTV) definition

For BT1 and BT4 the CTVstandard based on GTVct data and clinical pelvic examination was defined by radiation oncologist first; then the CTVstandard was reviewed with the inclusion of GTVpet data. The final CTV obtained from the overlap of CTVstandard and GTVpet data was called CTVPET-influenced. For the 2nd, 3rd, 5th and 6th BT fraction only the usual CTVstandard was contoured.

Statistical analysis

GTVpet, CTVstandard and CTVPET-influenced were recorded as absolute values in the F1 and F4 groups respectively. Mean ± standard deviation and range were used to describe these continuous variables. The difference between CTVstandard and CTVPET-influenced were analysed as absolute and percentage values. We compared CTVstandard and CTVPET-influenced with the non-parametric sum rank test and p-value of 0.05 was considered for statistical significance. A linear regression was applied to evaluate the relation between the different ways of contouring volumes and the Pearson coefficient was considered to summarize the goodness of the model. Stata software 9.0 (Stata Corporation, College Station, Texas, USA) was used for performing statistical analysis.

Results

All the patients enrolled into this study completed the protocol described above but out of 26 attempts of double CTV definition, only in 21 cases we were able to make a comparison between CTVstandard and CTVPET-influenced. In fact for two patients (n.6 and n.7) with PET completely negative at first and fourth BT only CTVstandard was defined (no informations added from PET). Patient n.3 on BT4 had an uptake in PET images too far from the applicator to be included in the treatment volume, and CTVPET-influenced was considered inappropriate for BT.

The average volumes obtained in each fraction are summarized in Table 2 and details are presented in Table 3.

<table>
<thead>
<tr>
<th>Age (y)</th>
<th>(55 ± 11) y</th>
<th>Range: 32-88 y</th>
</tr>
</thead>
<tbody>
<tr>
<td>Clinical FIGO Stage</td>
<td>3/13 (23%) IIA</td>
<td>1/13 (8%) IB</td>
</tr>
<tr>
<td></td>
<td>2/13 (15%) IIB</td>
<td>7/13 (54%) IIIB</td>
</tr>
<tr>
<td>Histology</td>
<td>13/13 (100%) Squamous Carcinoma</td>
<td></td>
</tr>
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</table>

Table 1: Characteristics of 13 patients enrolled into the study.
**Table 3:** Volume (ml) of GTV PT, CTV standard and CTVPET-influenced observed at first and fourth fraction of brachytherapy treatment (BT1 and BT4), differences (%) between CTV standard and CTVPET-influenced (absolute value in ml and percentage normalized at the average value of two CTVs) and Volume*PET (absolute value in ml and percentage normalized at CTV standard), that is the volume of GTVPET that does not intersect with CTV standard.

In the 21 cases the absolute difference between the two volumes ranged from 0.6 to 16.4 ml. The percentage of difference between the two volumes was normalized at the average value of the two CTVs. In 3/21 (14.3%) cases the difference between the two volumes was inferior to 5%, in 3/21 (14.3%) the difference was between 5% and 10%, in 3/21 (14.3%) cases the difference was between 10% and 20%, and in 12/21 (57.1%) the difference was >20%. In 5/21 cases (23.8%) CTVPET-influenced was greater than CTV standard while in 16/21 cases (76.2%) were lower than CTV standard.

**Analysis of volumes intersection**

In order to evaluate the impact of F18-FDG-PET/CT in defining brachytherapy volume, we have also considered the three-dimensional relative position of the volumes divided into six group (Group A-F Table 3). In 4/26 cases (Table 3: group A) GTVPET introduced major variations of the volume of irradiation; because PET/CT detected an uptake area undetectable by clinical visit or CT. The mean absolute value of GTVPET that did not intersect with CTV standard in these four cases was 7.65 ml. The mean percentage of GTV PET that did not intersect with CTV standard was 31.6%. In 3/26 cases (Table 3: group B) PET/CT scan slightly modified the volume and the mean absolute value of GTVPET that did not intersect with CTV standard was 1.07 ml. The mean percentage of GTV PET that did not intersect with CTV standard in these three cases was 4.0%.

In 6/26 cases (Table 3: group C) the uptake areas detected by PET/CT were not covered completely by the applicator's position because too far from the applicator. The stiffness of the applicator is a constructive factor that may not permit to adequately cover the metabolic area with a hypothetical isodose distribution. In these cases, the mean absolute value of GTVPET that did not intersect with CTV standard was 6.62 ml.

**Quantitative comparison of the volumes (CTV standard vs CTV PET-influenced)**

In the 21 valuable cases, the mean ± SD CTV standard for the BT1 and for BT4 were 27.9 ± 9.6 ml (range: 15.9-52.3 ml) and 23.5 ± 3.3 ml (range: 20.4-30.2 ml) respectively. The mean ± SD CTV PET-influenced for the BT1 and for BT4 were 22.8 ± 12.6 ml (range: 10.4-57.1 ml), and 20.2 ± 4.6 ml (range: 13.3-29.0 ml) respectively. Considering both fractions together, the mean ± SD CTV standard were 25.8 ± 7.5 ml and the mean ± SD CTV PET-influenced were 21.6 ± 9.5 ml. The difference between the two values is statistically significant with the sum rank test (p=0.01).
mean percentage of GTV$_{PET}$ that did not intersect with CTV$_{standard}$ (normalized at CTV$_{standard}$) was 23.6%.

In 8/26 cases (Table 3: group D) the metabolic positive area was nearly included into the CTV$_{standard}$, without additional information by PET/CT. However, the GTV$_{PET}$ did not matched with the CTV$_{standard}$ because the uptake was located in a area smaller than CTV$_{standard}$ in all these eight cases. In this subgroup the mean absolute value of GTV$_{PET}$ that did not intersect with CTV$_{standard}$ was 0.53 ml. The mean percentage of GTV$_{PET}$ that did not intersect with CTV$_{standard}$ (normalized at CTV$_{standard}$) was 2.4%.

In 1/26 cases (Table 3: group E) the GTV$_{PET}$ was considerably larger than the tumour zone identified by CT scan. The CTV$_{PET-influenced}$ was majorly modified by PET/CT data, but whole uptake area could not be irradiated because of the limits of the applicator.

In 4/26 cases (Table 3: group F), PET scan was negative without evidence of pathological FDG uptake in the cervix.

The different volumes identified by CT and by PET did not overlap in any case.

For the linear regression test, the correlation coefficient is equal to R$^2$=0.546 for the 21 data points (Figure 1).

**Outcome**

At 3 months after completion of the treatment, all the patients but one underwent a PET/CT which was totally negative for all of them. These are preliminary clinical data with a median follow up of 47 months (SD ± 14 months) 10/13 patients are alive, free from disease. Patient n.6 died for intercurrent disease at 3 months from the end of BT. For this patient PET at first and fourth fraction of BT were negative (Table 3: group F).

Two patients had distant failure without pelvic recurrence: patient n.3 (Table 3: group: E-C) had metastasis (lung and peritoneum) after 10 months from the end of BT treated with chemotherapy (DFS 10 months and OS 51 months); patient n.13 (Table 3: group C-B) died for rapidly progressive metastatic disease (bone and Only one patient lomboaortic lymph nodes) after 28 months from the end of the BT (DFS 26 months and OS 28 months). In 11 cases (Table 3: group D) had a local recurrence (cervix) at 11 month from the end of BT: she was rescued with surgery (DFS 11 month and OS 37 months). The median DFS and OS for all the patients are 44 and 47 months respectively. Acute GI toxicity GI (RTOG) was recorded, no late GU toxicity was observed.

**Discussion**

In cervical carcinoma the tumour volume is one of the most important prognostic factors [5-7]. Brachytherapy is an essential component of definitive radiotherapy of cervical cancer and nowadays needs the integration of 3D imaging: MRI is currently considered the best choice to define the reference volumes according to (GYN) GEC-ESTRO recommendations (2006) [15,18]. PET has been considered useful in radiation treatment of cervical cancer, to measure accurately the volume [22], to evaluate tumour volume changes during radiation therapy and to early discriminate good versus bad responders [26,27]. With these new techniques it seems possible to identify individualized volumes for each patients and in theory, for each fraction, to try an improvement of the outcome while reducing the toxicity. Only few dosimetric studies have been conducted about the use of PET in BT planning with similar results. Malapaya [10] compares 2D conventional treatment planning with 3D PET-based treatment planning suggesting that the spread of tumor as shown by PET could make a better coverage of the tumour volume. Lin et al. [23,24] showed that PET-based treatment planning can improve dose coverage without increasing toxicity.

In a more recent feasibility study the Authors reported better results by using PET/CT scan plan than conventional point A [25].

We compared the standard CT-based and the PET/CT-based clinical target volume (CTV) in BT planning to evaluate the role of functional imaging during BT plan in a cohort of patients who were treated under standard conditions.

Comparing the two volumes the percentage difference higher than 20% between CTV$_{standard}$ and CTV$_{PET-influenced}$ was in 57% of the total patients. We found some variable information from PET, in part coherent with clinical and CT data set, in part not coherent; also negative PET in 4/26 studies were found. The absence of FDG uptake in these women could be explained by the early effects of previous EBT: although these data could be of interest for the prognosis of the patients, so far we do not know how this information may be used in the treatment planning. Considering all other cases with a positive PET/CT scan, we observed a statistically significant difference between CTV$_{PET-influenced}$ and CTV$_{standard}$ considering the mean value of both fractions (Table 2). Our results suggest that a correlation between the two tumour descriptions shows some discrepancies.

In 8 cases the GTV$_{PET}$ was included into the CTV$_{standard}$, indicating that the two sets of information are coherent but PET information may be only used for an hypothetical adaptive BT. In the other cases, the GTV$_{PET}$ was not congruent with clinical pattern and CT information. In these cases the area of FDG-uptake could suggest the opportunity to modify the target volume. Patient n.3 had a PET/CT post treatment negative and no recurrence in pelvis was found even if during the two fractions of BT she had at the BT1 an uptake very extended (86.4 ml) and so it was impossible to cover the entire volume of GTV$_{PET}$. In a similar situation, according only to the PET information unless a very serious toxicity, we should have to consider a boost of external beam treatment instead of brachytherapy. At BT4 we observed a decrease in the FDG-positive volume but the uptake area was too much lateral and it cannot be reached from the applicator's position. Theoretically these may be considered a very important strategic information. This patient had a progression of disease (peritoneum and lung) treated with chemotherapy but no evidence of disease in pelvis.

In our small patient population, PET information in BT fractions were variable, sometimes suggesting the opportunity to modify the volume to be treated, sometimes congruent with clinical examination and CT information, sometimes negative and sometimes with residual tracer uptake areas often located to far from the applicator and very difficult, if not impossible, to include in the BT planning suggesting another technique of the treatment.

In our limited experience PET scan cannot be used to define target volume as the only source of information but needs integration; nevertheless our results confirm the feasibility of this protocol.

**Conclusion**

Because the different possibilities with added PET informations during BT plan, it is very difficult, in our experience, to identify the role of PET in radiation treatment planning of the cervical carcinoma in the phase of intracavitary brachytherapy. But we must consider the
integration of information as an opportunity for the future for a much more individualized treatment.

References


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