

A Formulation, Optimization and Evaluation of Controlled Released Alginate Beads Loaded-Flurbiprofen

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Abstract

While flurbiprofen (FLB) may cause local gastrointestinal problems such as sensation of warming or burning in mouth and stomach, it is recommended to be limited its therapeutic uses or use it as a modified-release preparation for only once daily-use using Calcium-alginate (Ca-alginate) beads. Ca-alginate beads were prepared by dropping sodium-alginate solution containing FLB into calcium chloride solution. The prepared Ca-alginate beads loaded-FLB were characterized by optical-microscope at different positions. The weight and swelling percent of the beads were measured for freshly and dried prepared beads. The release of the formed beads was studied in different releasing medias. Finally, after optimizing all conditions the formed beads were used to reduce the paw edema as an anti-inflammatory dosage form. The release of FLB from the formed beads in a phosphate buffer (0.2 M, pH 7.4) was slow and complete due to the FLB solubility at this pH. Kinetic analysis of the release-profile of FLB from the formed beads was obeyed the diffusion mechanism. The post carrageenan injection showed reduction of swelling in groups treated with Ca-alginate beads loaded-FLB with longer duration compared with the free FLB. The results showed that a simple and evaluated method for preparation of a modified-release Ca-alginate beads loaded-FLB for release for controlling of FLB with therapeutic purposes.

Keywords: Flurbiprofen; Modified-release preparation; Sodium alginate; Calcium alginate bead

Introduction

Flurbiprofen (FLB) a propionic acid derivative is a non-steroidal anti-inflammatory drug (NSAID), used in the treatment of mild to moderate pains such as dysmenorrhea, migraine, and musculoskeletal. The oral doses of FLB are usually large daily divided doses (from 150 to 200 mg) and may be increased to 300 mg as in acute or severe conditions if necessary. As NSAIDs, FLB may be cause local gastrointestinal problems such as the sensation of warming or burning in the mouth and stomach, therefore it is recommended to be limited the use of FLB to a few days of treatment or use a modified-release preparations for only once daily-use [1]. Pharmacokinetically, FLB is readily absorbed from the gastrointestinal tract after the mentioned oral dose. 99% of FLB is bound to plasma proteins, the peak plasma concentrations occur after 1 to 2 hr and its plasma half-life of 3 to 6 hours after administration [1,2].

Alginic acid is an unbranched polymer of β -D-mannuronic acid (M) and α -L-guluronic acid (G) linked by 1-4-glycosidic linkages. Alginates form a hydrogel in the presence of certain divalent cations such as calcium (Ca^{2+}) ions. The gelling characteristics of alginates are influenced by the uronic acid composition and the MM/GG (mannuronic acid block/guluronic acid block) is an index of the nature of the gel that is formed in the presence of the divalent cations [3,4]. Ca-alginates have attracted much attention of the formulators as a potential device for controlling drug release. They have many advantages such as protection the stomach mucosa from the irritant drugs or protects the acid-sensitive drugs from gastric juice, the re-swelling process of xerogel (gel after drying) in the intestine offers a controlled-drug delivery, as well as their non-toxic orally administration [5-7]. Alginates are characterized by its re-swelling behavior which envisages the following advantages; acid sensitive drugs are protected from gastric juice, the re-swelling process of xerogel (gel after drying) in the intestine offers controlled-drug delivery. Alginate is known to be non-toxic when taken orally, it protects the mucosa of stomach from irritating drugs [7]. The amount of drug released from the beads at pH 1.5 was relatively low which help in protecting the stomach from gastric irritation, whereas

the release reaches to 99% at pH 6.8. The drug can be encapsulated in nano-vesicle or micro-vesicle for local and systemic effect [8,9]. It was reported that, the released nifedipine and verapamil from the coated beads was minimal at pH 1.5 (18%), whereas approximately 99% nifedipine and verapamil was released at pH 6.8 [7,10]. Encapsulated nanoparticles or microparticles can be used for targeting certain site in the body [11-13]. The objective of this work was to utilize the alginate beads formulated with free FLB as a modified-release preparation for a few-daily usage to overcome the mentioned problems accompanied with FLB. The formed beads release FLB at pH 7.4, while can hold the FLB at pH 1.2 which serve in protecting the stomach from the irritating effect of FLB.

Materials and Methods

Materials

All chemicals and reagents used were of pharmaceutical reagent grades and some of them were used as such without any further purification. FLB standard powder (Boots Co., Nottingham, U.K.) was kindly supplied by Al-Kahira pharmaceutical Co., Cairo, Egypt. Sodium alginate (Na-alginate), Carrageenan, Urethane, and calcium chloride (CaCl_2) were purchased from Sigma Chemical Co. (California, U.S.A.). Potassium chloride (KCl), hydrochloric acid (HCl), sodium hydroxide (NaOH), acetic acid (CH_3COOH), and potassium dihydrogen

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Received January 06, 2016; Accepted February 19, 2016; Published February 22, 2016

Citation: Abdellatif AAH, El Hamd MA, Saleh KI (2016) A Formulation, Optimization and Evaluation of Controlled Released Alginate Beads Loaded-Flurbiprofen. J Nanomed Nanotechnol 7: 357. doi:10.4172/2157-7439.1000357

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orthophosphate (KH_2PO_4) were purchased from El-Nasr Chemical Co. (Cairo, Egypt). A male Albino rats (weight 120-200 g) which used in the present study were obtained from Animal House, Assuit University (Assuit, Egypt). (Assuit University animal care use committee) permitted the animal procedures in this experiment. Spectrophotometric measurements were made using an UV-1601 spectrophotometer (Shimadzu, Kyoto, Japan) with two matched quartz cells.

Experimental design

Preparation and evaluation of Ca-alginate beads loaded flurbiprofen: The Ca-alginate beads were prepared by dropping Na-alginate solution which is 2 gm Na-alginate in 100 mL water and containing 100 mg of FLB on 100 mL solution of 0.2 M CaCl_2 as reported previously [14,15]. The final homogenized solution filled into a 50 mL plastic syringe and dropped into a beaker containing 100 mL of CaCl_2 (by the aid of stirring) until the Ca-alginate beads loaded-FLB is spontaneously formed. For purification, the leached water was removed; the beads were washed with distilled water three times and then dried in an oven at 40°C for 12 hr. The dried beads were stored in a tightly closed glass container to avoid the moisture and humidity.

Ultraviolet spectroscopy: UV spectroscopy was used for determination of drug content and the amount of drug released from beads. Briefly, into a calibrated 500 mL stoppered conical flask, 100 mg of the formed beads added and stirred with 500 mL of phosphate buffer (0.2 M, pH 7.4), mixed well by stirring overnight. 1 mL of this solution measured spectrophotometrically at 247 nm. Then the actual drug concentration was calculated as:

$$= \text{Absorbance} \times \text{proedural constant} \times 500/1000$$

Differential scanning calorimetric (DSC): The effect of CaCl_2 molar concentration and drug: alginate ratio (D: P) using a fixed concentration of CaCl_2 solution, 0.2 M on the diameter of the formed alginate beads was studied. DSC studies were carried out to confirm the obtained Ca-alginate D: P ratio, as well as the untreated drug, which indicated the extent of crystallinity of the drug in presence of the studied alginate. Two states were studied, the beads which prepared in different concentrations of CaCl_2 and the effect of the different D:P ratios (using one CaCl_2 , 0.2 M). This method of analysis in as accordance of other results reported previously for other formula.

Characterization of the Ca-alginate beads loaded flurbiprofen: The diameter of the formed beads was determined with an optical-microscope at different positions and then the mean diameter of ten beads was calculated. The weight of the beads was determined as their water contents by weighing ten beads before and after drying, the average weight of ten beads was determined as the mean of five determinations and calculated as:

$$\text{Water content, \%} = \frac{\text{weight before drying} - \text{weight after drying}}{\text{weight before drying}}$$

The swelling percent (swelling percentage) of the dried beads was carried out in different medias (having different pH) such as distilled water, 0.1 N HCl (because it mimics the gastric pH of 1.2) and phosphate buffer (0.2 M, pH 7.4). Thirty beads were placed into 500 mL of the medias and rotating (50 rpm) for (6 hr) at 37°C. Three beads were taken out periodically and the diameter of each was measured at three different positions. The swelling percentage was expressed by the ratio of the average of these diameters of dried beads/average diameters of wetted beads [16]. The diameter of the formed beads before and

after drying was performed using an optical microscope with power of microscope 100. The size and shape of the beads were drowning by putting a white paper and drawing the surface of beads using the background of the beads.

In vitro release and kinetic analysis of flurbiprofen from Ca-alginate beads loaded flurbiprofen

The release of alginate beads (CaCl_2 , 0.2 M at 1:1 ratio) was studied in these medias and the study was focused on the release of FLB from alginate bead in phosphate buffer (pH 7.4) prepared using different concentrations of CaCl_2 solution or at fixed phosphate buffer (0.2 M) and different ratios [17]. In these studies, a rotating basket apparatus method was utilized. An accurately weighed amount of Ca-alginate beads equivalent to 50 mg of FLB was placed in a basket of USP validate-dissolution tester pre-filled with a dissolution medium (500 mL of each) and rotating (50 rpm) for time at 37°C. 1 mL of sample was withdrawn, periodically, diluted with appropriate volume of phosphate buffer (Beer's law between 0.1 and 1.0) and finally measure at 247 nm. The removed samples were replaced with the same amount of phosphate buffer (pH 7.4) [18,19]. The released percentage was plotted against the square root of time, the slope and the Y-axis intercept can be deduced from such relation. The slope of this plot is a quantitative measure of the rate of drug release in cases when diffusion mechanism operates. The effect of different molar concentrations of CaCl_2 and also the effect of D:P ratios (at CaCl_2 , 0.2 M) was checked to determine the diffusion rate constant (K_p).

Evaluation of anti-inflammatory activity of beads loaded flurbiprofen: The anti-inflammatory activity of beads was checked by applying the method of carrageenan induced rat's paw edema [20]. Briefly, thirty-six male Albino rats were used; they randomly allocated to six groups each consists of six rats. Group I is control, group II is free alginate (blank), group III and IV are free FLB, and group V and VI are the formed beads-FLB. After animals were fasted overnight, they had given 3 mL of water (to reduce the variability to edema response) before the administration test of free alginate beads (blank beads), free FLB, and formed alginate beads loaded-FLB (30 mg/kg), the dose was chosen according to the previously reported results [21]. The rats were anesthetized with Urethane (1.2 g/kg, intraperitoneal). Each group was received the specified formula through a special gastric incubation into the esophagus (in a dose equivalent to 20 mg/kg), followed by administration of the selected formulae. After 2 hr of formulae administration, 0.1 mL of carrageenan solution (1%, w/v) was injected subcutaneously into sub-planator tissue of one hind paw to induce the inflammation. The thickness of the paw edema was measured using a micrometer, and determined before and immediately after injection of carrageenan. Subsequent measurements were carried out at 1, 2, 3, 4, 5 and 6 hr after induction of edema. The anti-inflammatory effect was expressed as an inhibition percentage of edema thickness compared with control group according to the following equation.

$$\text{Inhibition of edema, \%} = \frac{T_0 - T_t}{T_0} \times 100\%$$

Where, T_0 is the edema thickness in control group, T_t is the edema

thickness in treated group. Then the obtained results were tested for a significantly difference by using one-way ANOVA test in SPSS software package (version 9).

Results and Discussion

As previously reported, sodium alginate is dropped to a solution of calcium chloride, a gel formed as the sodium ions was exchanged with calcium ions and the polymer cross-linked together. When the alginate is longer in contact with the calcium chloride solution, more rigid gel will become and more cross-links with the calcium ions can be formed [14-15].

Differential scanning calorimetry study

In order to shed a light on the possibility of solid-state changes of FLB with alginate polymer, DSC was performed on the individual components and the physical mixture of beads. The DSC curve of the untreated FLB and the free sodium alginate shows an endothermic peak at 113.3°C and 250.3°C, respectively at a scanning rate of 10°C /min. The DSC thermogram of the obtained Ca-alginate blank beads shows no endothermic peak at 250.3°C. While, The thermogram of alginate beads loaded-FLB, at 1:1 ratio and dropped in 0.2 M of CaCl₂, shows two endotherms at 250.4°C and 114.2°C with energies of 16.1 J/g and 81.0 J/g, respectively. The endothermic peak of the drug exists at the same position compared to the untreated drug (113.3°C), Figure 1A. The same results were obtained with FLB alginate beads at 1:0.5 ratio and dropped in CaCl₂, 0.2 M, but the endothermic peak of the drug and polymer with low distinct sharpened appearance than the former type which indicates that there is no interaction between the drug and the polymer as shown in Figure 1B.

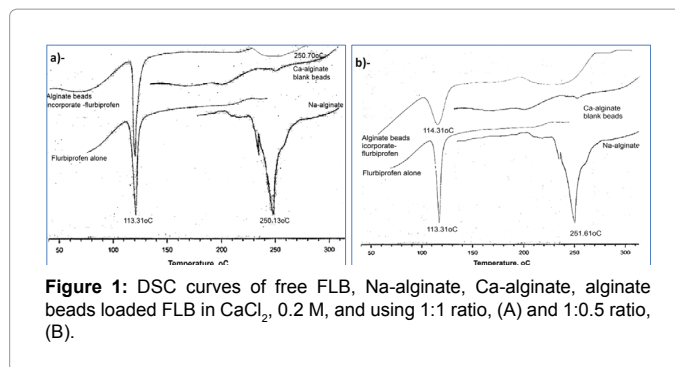
Characterization and evaluation of Ca-alginate beads loaded flurbiprofen

The formed alginate beads had big sizes and heavy weights before drying as they hold an amount of water about 94% calculated after drying, Table 1. This amount of water aided in the formation of spherical beads with smooth surface as shown in Figure 2. The size and weight was decreased significantly of dried beads, due to the loss of water of about 0.30% in the beads.

Microscopic examination of Ca-alginate beads

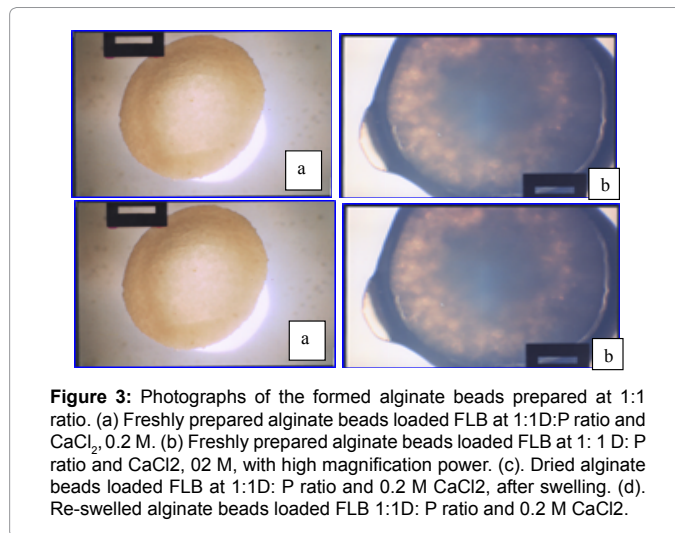
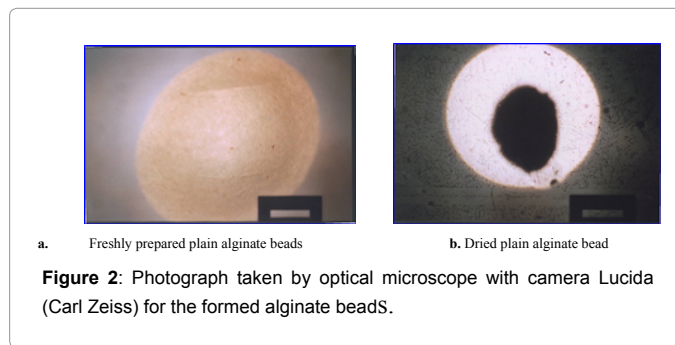
A freshly prepared spherical-shape Ca-alginate bead before drying is shown in the photomicrographs, Figure 2A. Gelation seemed to occur instantly on the surface of the droplets forming almost spherical beads without splashing of the fallen droplets (distance of fallen droplets was 20 ± 5 cm). Figure 2B shows a dried plain alginate bead which became less spherical and their size decreased significantly. Figure 3 shows the shape and the surface of beads at 1:1 ratio. The beads are spherical with granulated surface. The crystals seen on the surface could be formed during drying due to insolubility of the drug and the shrinkage of alginate beads. Where, the loaded drug was greater, the crystals seemed with bigger size covered by the alginate. Hence, the beads cover appeared to be improved when the matrices were produced from a more concentrated drug suspension at the same time, fissures appeared clearly with the increased the alginate content.

The effect of CaCl₂ concentration on the diameter of the formed alginate beads and the effect of D: P ratios at a fixed CaCl₂ solution were studied. The data in Table 2 revealed that the alginate beads diameter increases as the molar concentration of CaCl₂ decreases. It was obvious that, the beads were shrunk significantly during drying and had a small size (diameter ≈ 1.32-1.78 mm). Less shrinkage with bigger beads size was observed with either increase in amount of loaded (loaded) FLB or with decrease for CaCl₂.



Beads Property	Before drying	After drying
Diameter, mm	2.22 ± 0.07	0.808 ± 0.04
Weight, mg/bead	7.55 ± 0.21	0.418 ± 0.01
Water content	94.46%	(0.30%)

Table 1: Physical properties of plain Ca-alginate beads loaded-FLB before and after drying



Swelling percentage of Ca-alginate beads loaded flurbiprofen

FLB powder is sparingly soluble in water at low pH values but readily soluble in pH above 7 [22]. The swelling percentage and consequently the release efficiency are necessary to be checked in a different medias having different pH. However, the swelling percentage of Ca-alginate beads in phosphate buffer was greater than its original size through 1-1.5 hr. The disintegration and dispersion are gradually occurring over more than one hr. Furthermore, the matrices remained intact in spite

(A) Molar concentration of CaCl ₂ (1:1 ratio)	Diameter of beads, mm		Weight of beads, mg	Loaded-FLB, (mg)	Encapsulation efficiency, percentage
	before drying	after drying			
0.025	2.6 ± 0.1	1.6 ± 0.1	0.7 ± 0.0	49.4 ± 0.5	98.7
0.05	2.1 ± 0.1	1.6 ± 0.1	0.6 ± 0.0	45.7 ± 0.5	91.3
0.1	2.2 ± 0.1	1.5 ± 0.1	0.6 ± 0.0	43.8 ± 0.5	87.6
0.2	2.1 ± 0.0	1.4 ± 0.2	0.6 ± 0.0	42.6 ± 0.6	85.2
0.5	2.0 ± 0.3	1.4 ± 0.0	0.5 ± 0.0	36.6 ± 0.5	73.5
1.0	20.0 ± 0.1	1.3 ± 0.1	0.6 ± 0.0	33.1 ± 0.5	66.1
(B) D:P ratios	Diameter of beads, mm		Weight of beads, mg	Loaded-FLB, mg	Encapsulation efficiency percentage
	before drying	after drying			
1:0.5	2.8 ± 0.1	1.8 ± 0.1	0.6 ± 0.1	49.3 ± 0.5	98.5
1: 1	2.6 ± 0.1	1.6 ± 0.1	0.7 ± 0.1	45.6 ± 0.5	91.3
1 : 2	2.7 ± 0.1	1.5 ± 0.1	0.6 ± 0.1	42.5 ± 0.5	84.9
1 : 3	2.7 ± 0.1	1.6 ± 0.1	0.7 ± 0.1	41.1 ± 0.5	82.1
1 : 4	1.8 ± 0.1	1.4 ± 0.1	0.5 ± 0.2	35.2 ± 0.5	70.2
1 : 5	2.1 ± 0.1	1.3 ± 0.1	0.5 ± 0.1	29.9 ± 0.5	59.8

Table 2: Characterization of Ca-alginate beads, prepared in different concentrations of CaCl₂, at 1:1 ratios (A); and their characterization after preparation in CaCl₂, 0.2 M at different D: P ratios (B).

of conversion of Ca-alginate beads to alginic acid having a transparent appearance. Figure 4 shows the difference in the swelling percentage of Ca-alginate beads in these media.

In vitro release of flurbiprofen from the Ca-alginate beads loaded flurbiprofen

Most of the release data were shown to follow diffusion-controlled mechanism [23,24]. The release profile of loaded-FLB from the alginate beads in water and in 0.1 N HCl pH 1.2 was showed in Figure 5. The release demonstrates a high retardation of FLB from alginate beads. Only 3.6% and 4.8% of drug content in the beads were released after two hr in water and 0.1 N hydrochloric acid pH 1.2, respectively. The low release of FLB indicates that alginate beads could serve as reservoir for FLB release prolongation.

The release-profile of FLB from alginate beads prepared using different concentrations of CaCl₂ was slow compared with plain drug, this is due to low solubility of FLB as well as the slight swelling of alginate in the phosphate buffer. Alginate beads with a higher concentration of Ca²⁺ ions demonstrated a slower rate and lower extent of drug release. While, alginate beads prepared in CaCl₂, 0.025 M (1:1 ratio) has a high release rate and high drug loaded (Figure 6). Next, the results revealed that the release rate was relatively faster with the increase in alginate contents. Figure 7 shows the effect of different ratios of D:P on the release-profile of FLB from the formed alginate beads, when prepared in CaCl₂, 0.2 M. Alginate beads prepared at 1: 0.5 ratios shows a high release rate and high incorporating-drug. While alginate beads prepared at 1: 5 ratio shows a low drug release and low incorporating-drug. As the result shows the alginate beads prepared at 1: 1 ratio in CaCl₂, 0.2 M was used for the further studies as the best type of beads as it have a moderate release rate and moderate drug loading.

Kinetic analysis of release-profile of flurbiprofen from the Ca-alginate beads loaded flurbiprofen

The diffusion matrix results are shown in Table 3 for release percentage data was obeyed the diffusion mechanism, these data were supported by previously results [25]. The results were revealed, the K_h (while the other parameters were fixed) from CaCl₂ beads 0.025 and 0.05 M was 4.048 and 4.176/min. Further increase the concentration of CaCl₂ from 0.1 M to 1 M, decreased the value of K_h from 3.904 to 3.639/min. while, increasing the polymer ratio in D:P ratios (from 1:0.5 to

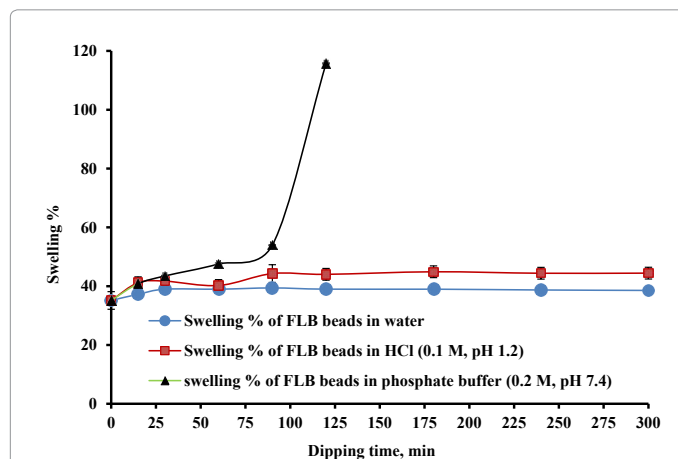


Figure 4: Swelling percentage of FLB beads, in water, in HCl (0.1 M, pH 1.2) and in phosphate buffer (0.2 M, pH 7.4).

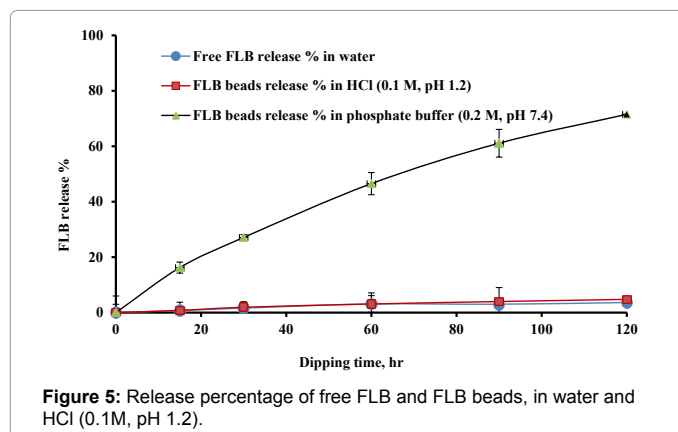


Figure 5: Release percentage of free FLB and FLB beads, in water and HCl (0.1M, pH 1.2).

1:5) increased the value of K_h from 4.211 to 4.66/min.

Evaluation of anti-inflammatory activity of Ca-alginate beads loaded flurbiprofen

The result in Figure 8 illustrates the anti-inflammatory effect of free

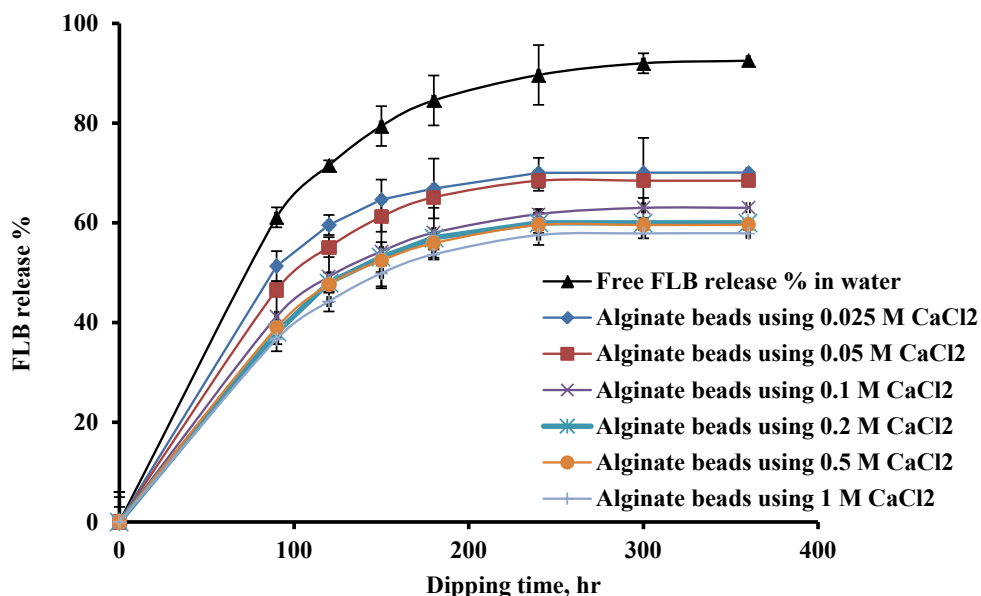


Figure 6: Release percentage of FLB beads in phosphate buffer (0.2 M, pH 7.4) using different concentration of CaCl₂ (at 1:1 ratio).

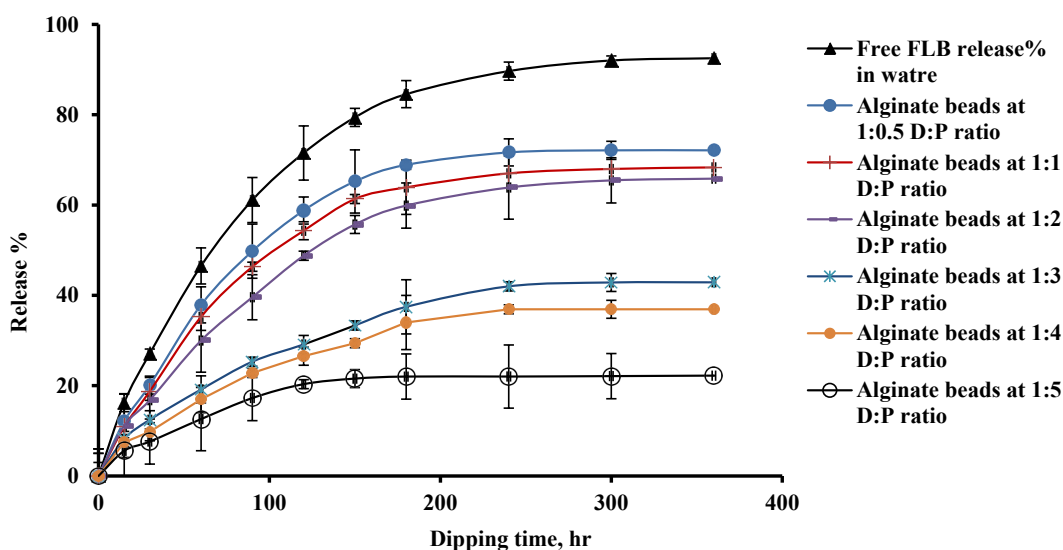


Figure 7: Effect of different D: P ratio on the release percentage of FLB beads in phosphate buffer (0.2 M, pH 7.4) using CaCl₂ (0.2 M).

alginate beads, free FLB, and alginate beads loaded-FLB. It is obvious that at 1 hr post carrageenan injection, there is apparent reduction of swelling in groups treated with alginate beads loaded-FLB (V, VI), and free drug (groups III, IV) compared with the control group (group I). There is no evident inhibition in edema swelling in group II.

The inhibition percentage of edema swelling using the group V, VI, and group III, IV, were 12.3 and 14.1 versus 6 for the group II. After 2 hr post carrageenan injection the anti-edema effect was higher in group V, VI, and groups III, IV, where the inhibition% of edema swelling was 23.1, and 33 versus 1.84 into group II. After 5 hr post carrageenan injection the anti-edema effect of alginate beads loaded-FLB was higher, where the inhibition percentage of edema swelling was 51.9 versus 18.12 in

group III, IV. Next, 6 hr post carrageenan injection groups V, VI, still exhibited a significant inhibition of the carrageenan induced edema, which is numerically higher than that observed in the rats in groups II or III, IV, where the inhibition percentage in edema swelling was 41.4 versus 2.71 and 6.7 in groups II and III, IV respectively, as shown in Figure 8.

Table 4 shows the statistical analysis (correlation bivariate two tailed analysis) of control, blank alginate beads, and alginate beads loaded-FLB. The correlation is significant different at probability levels, 0.05 and 0.01. The significant results are 0.93 and 0.80, respectively.

One-way ANOVA test of inhibition percentage in rat paw edema of control, blank alginate beads, and alginate beads loaded-FLB is shown

(A) Mechanism of release		Different CaCl ₂ concentration, M					
		0.025	0.05	0.1	0.2	0.5	1
1 st order	r	- 0.878	- 0.896	- 0.922	- 0.866	- 0.896	- 0.917
	K _r /min	- 0.001	- 0.001	- 0.001	- 0.001	- 0.001	- 0.001
Zero order	r	0.834	0.855	0.873	0.838	0.866	0.879
	K ₀ , release percentage /min	0.157	0.1637	0.154	0.148	0.146	0.144
Higuchi's diffusion	r	0.923	0.938	0.949	0.923	0.943	0.952
	K _h , release percentage /min	4.048	4.176	3.904	3.799	3.709	3.639
Log Q Vs. log t	r	0.952	0.957	0.964	0.959	0.953	0.969
	Slope	0.5805	0.448	0.467	0.497	0.536	0.475
Best fitted model		k _h					
(B) Mechanism of release		Drug: polymer ratios					
		1:0.5	1:1	1:2	1:3	1:4	1:5
1 st order	r	- 0.899	- 0.972	- 0.922	- 0.936	- 0.922	- 0.814
	K _r /min	- 0.002	-0.001	- 0.001	- 0.001	- 0.001	- 0.001
Zero order	r	0.853	0.977	0.873	0.897	0.907	0.805
	K ₀ , release percentage/ min	0.163	0.088	0.154	0.158	0.0878	0.045
Higuchi's diffusion	r	0.936	0.997	0.949	0.963	0.967	0.901
	K _h , release percentage /min	4.211	2.088	3.904	3.951	2.171	1.166
Log Q Vs. log t	r	0.981	0.915	0.964	0.981	0.983	0.951
	Best fitted model		k _h				

Table 3: Kinetic study of drug release percentage from FLB beads at different CaCl₂ concentration and 1:1D: P ratio (A); and Kinetic study of drug release percentage from alginate beads at CaCl₂ 0.2 M and different D:P ratios in phosphate buffer (25 ± 5OC) (B).

Factors	Control		Free alginate beads		Free FLB		Alginate beads loaded-FLB	
	r	Sign. ¹	r	Sign. ¹	r	Sign. ¹	r	Sign. ¹
Time, min	0.83	**	0.26	---	0.52	---	0.19	---
Control			0.12	---	0.30	---	0.43	---
FLB beads					0.38	---	0.54	---
Free FLB							0.99	**

¹Significant difference

Table 4: Statistical analysis of control, blank alginate beads and FLB beads on the carrageenan-induced edema in the hind paw of rats.

Dosage form		Summation of squares	DF ¹	Mean of square	F ²	Sign. ³
Free alginate beads	Between groups	7.82	4	1.95	0.99	0.63
	Within groups	1.98	1	1.98		
	Total	9.81	5			
Free FLB	Between groups	702.23	4	175.56	0.41	0.81
	Within groups	426.32	1	426.32		
	Total	1128.55	5			
FLB beads	Between groups	638.98	4	159.74	0.30	0.88
	Within groups	529.43	1	529.43		
	Total	1168.4	5			
Control	Between groups	17.98	4	4.51	0.84	0.67
	Within groups	5.38	1	5.38		
	Total	23.36	5			

¹DF: Dilution factor; ²F: F-value; ³sign: Significant difference.

Table 5: One way ANOVA test for inhibition percentage of rat paw edema.

in Table 5. The results obtained revealed that the selected alginate beads loaded-FLB have an anti-inflammatory activity with long duration of action.

Conclusion

In conclusion, the present study reveals the characteristics of FLB-loaded alginate bead formulations; drug loading, polymer percentage and the Molar concentration of CaCl₂ used influenced the encapsulation

efficiency and in vitro drug release characteristics of the prepared beads. Ca-alginate loaded-FLB, a macro-encapsulation delivery system was investigated for the solubility enhancement and improving the bioavailability of water insoluble FLB drug, using Ca-alginate beads formulae. Moreover, it is a novel method to prepare efficient anti-inflammatory FLB beads which able to mask the drug taste and its burring effect in the oral cavity and stomach. The gastro protective effect of flurbiprofen-loaded alginate beads was the main achievement

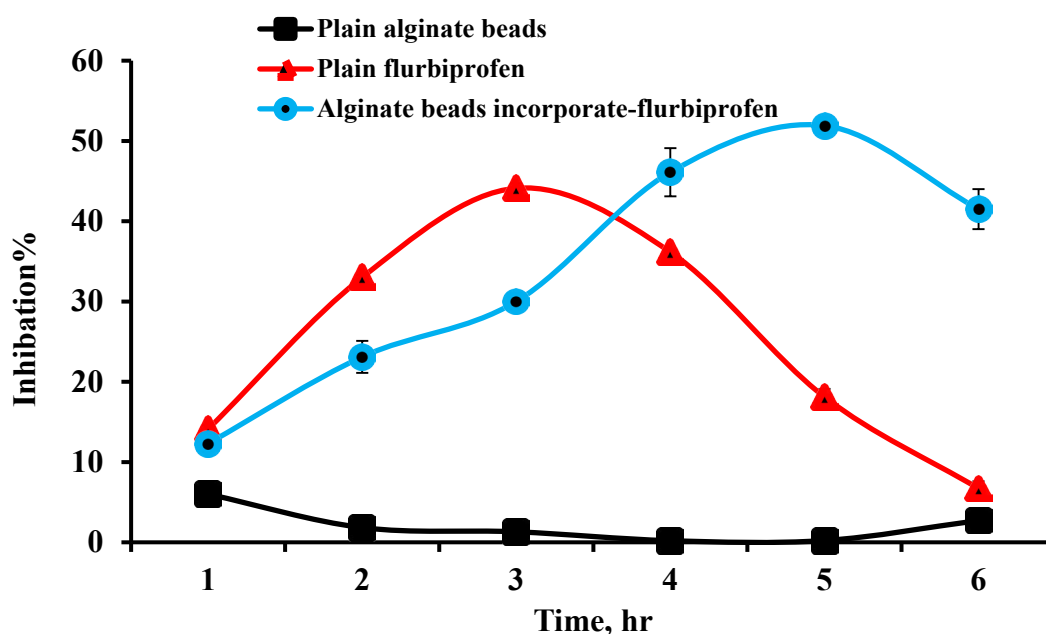


Figure 8: Inhibition percentage of rat paw induced edema for the selected formulae.

of this study. Therefore, these beads are promising pharmaceutical forms, which provide controlled-release drug delivery systems and covering the gastric effect of NSAIDs.

Conflict of Interest

Authors declare no conflict of interest.

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Citation: Abdellatif AAH, El Hamd MA, Saleh KI (2016) A Formulation, Optimization and Evaluation of Controlled Released Alginate Beads Loaded-Flurbiprofen. J Nanomed Nanotechnol 7: 357. doi:[10.4172/2157-7439.1000357](https://doi.org/10.4172/2157-7439.1000357)

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