Ab Initio Semi-Quantitative Analysis of Micro-Beam Grazing-Incidence Small-Angle X-Ray Scattering (M-GISAXS) during Protein Crystal Nucleation and Growth

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Abstract

Micro-beam Grazing-Incidence Small-Angle X-ray scattering (μ-GISAXS), exploiting both the advantages of elastic X-ray scattering and the highly focused third-generation synchrotron radiation micro-beams, is an advanced scattering technique that enables scientists to unravel the details of crystal growth processes and to investigate large-scale structures in thin films, including nanobiofilms or other different kinds of surfaces, such as surface gradients or confined surfaces.

In this study, we analyze semi-quantitatively and we simulate our previously acquired μ-GISAXS experiments of Thaumatin and Lysozyme Langmuir-Blodgett (LB)-film, shedding light on nucleation and crystal growth processes. Here, we show that, during LB-thin film facilitated nucleation, the particle radius of Thaumatin and of Lysozyme crystal increases while the film thickness reduces. Structural re-organization inside and within the LB-thin film are likely to lead to the crystal nucleation and growth. These semi-quantitative findings are in agreement with the model previously hypothesized. New insights and implications for protein nanocrystallography are also discussed.

Keywords: Ab initio semi-quantitative analysis; Crystal growth; Crystal nucleation; IgGISAXS; Langmuir-Blodgett (LB) nanobiobtemplate; Lysozyme; Micro-beam Grazing-Incidence Small-Angle X-ray Scattering-(μ-GISAXS); Thaumatin

Introduction

Protein crystallization is a challenging issue for solving and determining the crystallographic structures of molecules of crucial medical importance: it is a time-consuming, highly demanding task, characterized by many rate-limiting steps and bottlenecks [1-5].

Problems and difficulties due to the identification of the precise crystallization conditions and parameters [6] are often encountered in classical crystallography, despite its advancements and achievements [7].

In order to overcome these issues, in the last years we developed and proposed an approach termed as "protein nanocrystallography" or better "protein nanobiocystallography", in which nanobiotechnologies play a major role. Protein crystal nucleation and growth are facilitated and enhanced through a Langmuir-Blodgett (LB)-based nanobiomplate [8-14].

LB nanobiomplate enables scientists to finely manipulate molecules and proteins, and allows the development and design of highly ordered nanobiopatterns and sensitive nanobiensors [15-17].

In many investigations, we found that protein crystals grown on nanobiomplate surfaces exhibit very interesting features, such as thermostability [18,19], enhanced radiation resistance [20-22], unique water structure [23,24] and submon domains [25].

The growth of protein (such as, for example, Cytochrome P450sc, Thaumatin and Lysozyme) films on homologous crystal surfaces has been studied and characterized by Atomic Force Microscopy (AFM) [26-28], but microscopic details of the crystal growth process are still poorly known.

Grazing-incidence Small Angle X-ray scattering (GISAXS) is an advanced scattering technique that can be used to unravel these processes and to investigate large-scale structures in thin films, including biofilms [29,30].

A combination of this technique with third-generation synchrotron radiation micro-beams (μ-GISAXS) [31] has been used for studying different kinds of surfaces, like surface gradients or confined surfaces. The potential for studying thin protein films by μ-GISAXS during nanomplate-assisted crystallization experiments was previously demonstrated in a study about the effect of temperature on long-range order [19] and during both ex situ and in situ experiments [32-36]. Ex situ data obtained using both Cytochrome P450sc and Lysozyme were extremely complex to interpret and needed to be studied in parallel with microscopy characterization, using either the classical method or the nanomplate hanging-drop method [32,33], as well as in situ data [34-36]. Moreover, ex situ experiments were partially limited by the

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discontinuous nature of the studies themselves and for addressing this issue, \textit{in situ} experiments were carried out, designing an \textit{ad hoc} apparatus, namely the flow-through crystallization cell, which, besides the conventional crystallization set-up, is made up by two kapton windows being inserted into the outer cell walls (Figure 1) [35,37]. For obtaining a rapid and proper buffer exchange, the reservoir was connected via Teflon tubes to two Harvard syringe pumps. The main advantage of \textit{in situ} experiments was the possibility of monitoring the different processes of crystal growth in real time.

The aim of this work is to shed light on the processes of nucleation and crystal growth starting from a LB-protein film by semi-quantitatively analyzing previously acquired \textit{in situ} µ-GISAXS experiments with suitable models [34-36].

We want to stress and underline some limitations of our simulation analysis. The used model of cylinder is only a starting point of the analysis to grasp the main evolution of the morphology of the surface i.e. crystallites on a LB thin film. However, the process of protein crystallization and the corresponding morphology may be much more complex than this approximate picture of the surface roughness. This explains the difficulties of finding simultaneously the right power law decrease of the intensity along the two directions of space. On the other hand, even if preliminary, this work represents advancement in comparison with the only qualitative analysis we previously carried out. 

\textbf{Materials and Methods}

\textbf{Thaumatin crystallization}

Thaumatin I, a plant sweet protein from \textit{Thaumatococcus daniellii} (T7638, molecular mass 22 kDa) was purchased from Sigma Aldrich (Milan, Italy). Thaumatin protein monolayers were deposited onto glass slides by the Langmuir-Schaefer (LS) method, which enables to obtain a highly packed and ordered Thaumatin monolayer with a surface density of \(9.69 \times 10^{10}\) molecules/mm\(^2\), corresponding to \(10.32\) nm\(^2\)/molecule, which fits well with the molecule geometric features from the Protein Data Bank (PDB code 3DZR) and from AFM measurements of LS film [35,36].

The 100 ml of filtered (0.45-mm filter unit, Millipore, Carriagtwohill, Ireland) protein solution of concentration 1 mg/ml was spread onto the air-water interface of the Langmuir-Blodgett (LB) with a Hamilton syringe (Reno, NV).

Distilled water purified with a Milli-Q system (18.2 M\(\Omega\)-cm; standard protocol ISO 3696; Millipore, Billerica, MA) was used as sub-phase. The protein monolayer was compressed immediately after spreading to a surface pressure of 20 mN/m. Transfer of the protein monolayer from the sub-phase surface onto a solid support was performed by touching the support parallel to the sub-phase surface according to the LS technique (horizontal lift) at a fixed surface pressure. The crystallization conditions used for the modified hanging-drop method reported here, with two LB layers of Thaumatin, were as follows. A 4-ml drop containing 15 mg/ml of Thaumatin in 100 mM N-(2-Acetamido)iminodiacetic Acid (ADA) buffer, at pH 6.5, was mixed with 4 ml of the reservoir solution (1 M sodium/potassium tartrate in 100 mM sodium/potassium tartrate buffer, at pH 6.5) and placed on a siliconized glass slide in the classical method, or on a Thaumatin nanotemplate in the LB method, and stabilized over the reservoir containing 1 M sodium/potassium tartrate in 100 mM sodium/potassium tartrate buffer, pH 6.5 [35,36].

\textbf{Lysozyme crystallization}

Lysozyme (EC 3.2.1.17, of \textit{Gallus gallus}) was purchased from Sigma Aldrich (Milan, Italy). Lysozyme is a 15kDa protein of 129 amminoacids, that hydrolyzes different polysaccharides and has anti-bacterial properties. Lysozyme thin film was prepared on the water-area interface and compressed to a surface pressure of 25 mN m\(^{-1}\) by means of a LB trough. A protein monolayer was deposited onto a siliconized glass circle cover slide of 12 mm diameter (Hampton Research) by the LS technique (horizontal lift) at a fixed surface pressure. The droplet of protein solution and the precipitant (salt) was placed on the glass slide covered by thin film nanotemplate. As in the classical hanging-drop method, the glass slide with the protein template and the drop was sealed on the crystallization plate (Limbro plate, Hampton Research) using vacuum grease. The crystallization conditions usually used for the classical hanging-drop method were applied: a 6 µl drop containing 20 mg/ml Lysozyme in 50 mM sodium acetate buffer at pH 4.5 and 0.45 M sodium chloride was placed on the siliconized glass slide covered with the Lysozyme monolayer and stabilized over the reservoir containing 1.8 M sodium chloride in sodium acetate buffer for the first 20 minutes (accelerated nucleation) and 0.9 M up to the following 24 hours (controlled growth) [34].

\textbf{Experimental Thaumatin and Lysozyme µ-GISAXS}

\textit{In situ} scattering experiments were performed at the ID13
microfocus beamline facility at the European Synchrotron Radiation Facility in Grenoble, France [34-36]. μ-GISAXS is an advanced scattering method which allows investigating large-scale structures in thin film [38-40] but which requires brilliant and focused beam from a synchrotron source. The incoming monochromatic beam (\(\lambda = 0.991\ \text{Å} - 12.7\text{keV}\)) was focused by a set of two crossed Fresnel lenses on a spot of dimensions 0.5 x 1 \(\mu\text{m}^2\) (full width at half-maximum) at the sample position with a flux of \(-10^8\) photons/s. A micro-ionisation chamber with a 20 \(\mu\text{m}\) guard aperture was used to monitor beam intensity and to reduce parasitic scattering. The direct beam was blocked by a 300 \(\mu\text{m}\) diameter beam stop to avoid overexposure of the detector.

The flow-through crystallization cell (pictorially shown in Figure 1) was placed on a two-axis goniometer with rotating angle (\(\alpha, \psi\)), mounted on an x/y/z translation unit with the X-ray beam direction along the x-axis.

The crystallization cell set-up was tilted by the goniometer to adjust the fixed angle of incidence (\(\alpha = 0.71^\circ\)).

The μ-GISAXS pattern was recorded on a MAR165 CCD detector (2000 x 2000 pixels with a 78.94 x 78.94-mm pixel size; 16-bit readout). The sample-to-detector distance was 791 mm as determined by an Ag-behenate standard [41].

A typical μ-GISAXS pattern is indexed as function of the wave-vector transfer \(Q = (Q_x, Q_y, Q_z)\) which parallel \(Q_z\) and perpendicular \(Q_x\) components scale with the in-plane \(2\alpha\) and exit \(\alpha\) scattering angles [42]. Knowing \(\alpha\) is the grazing incidence angle, \(Q_x\) and \(Q_z\) can be computed as follows:

\[
Q_x = 2\pi/\lambda \sin(2\alpha)
Q_z = 2\pi/\lambda \sin(\alpha) \sin(\alpha)
\]

While \(Q_x\) is negligible in most conditions.

The specular and the so called Yoneda Peak [43] occur as characteristic features in the scattering pattern.

Real GISAXS patterns are shown in Figures 2 and 3 for Thaumatin and for Lysozyme, respectively.

A typical μ-GISAXS pattern of Thaumatin is shown in Figure 4 [35,36]. Specular scattering is observed for \(Q_z = Q_x = 0\), \(Q > 0\), with the specular peak appearing when the specular condition is fulfilled (\(\alpha = \alpha\)), and while diffuse scattering is observed for \(Q_x \neq 0\). The so called Yoneda Peak \(\alpha = \alpha\) occurs at the critical angle \(\alpha\) of the sample. Correlations vertical to the sample surface can be probed along \(Q_z\) at \(Q_x = 0\) [43].

For the LB-Lysozyme μ-GISAXS, which is shown in Figure 5, was acquired for 1 second at a time interval of 2 minutes in the first 30 minutes, while at 26 minutes the acquisition time was changed to 5 seconds [34]. Images were recorded up to a total of 93. For the classical Lysozyme, μ-GISAXS was acquired for 5 + 5 seconds at a time interval of 110 seconds from 30 minutes up to 3 hours; a total of 268 images were recorded.

The excluded area in Figure 5 takes into account only the sharp peak due to the reflected beam. The bump may arise from the interplay between the foot of the sharp peak and the surface roughness, which is difficult to model. But, as we previously stated and emphasized, the used-model of cylinder is only semi-quantitative and reproduces only the overall power law decay of the intensity.

Critical angles of Thaumatin, Lysozyme and glass for the used X-ray energy were calculated on the basis of their chemical formula and densities [44].

Data reduction

The Fit2D software package was used for data reduction [45]. GISAXS patterns were analyzed with the IsGISAXS software [46-].
which is dedicated to simulation of scattering from supported nanostructures. The scattering cross section is expressed in terms of island form factor and interference function and the specificity of the grazing-incidence geometry is stressed, in particular in the evaluation of the island form factor in the distorted-wave Born approximation (DWBA). A full account of size and possible shape distributions is given in the decoupling approximation (DA), where sizes and positions are not correlated, and in the local mono-disperse approximation (LMA). Two types of island repartitions on the substrate can be implemented: disordered systems characterized by their particle-particle pair correlation functions, and bi-dimensional crystalline or paracrystalline systems of particles.

**Choice of parameters**

The scheme adopted for ab initio data reduction is shown pictorially in Figure 1 and described in details in Gebhardt et al. [35,36].

In table 1, the parameters which have been used in our simulation for modeling the crystal growth have been reported. Proteins have been modeled as cylinders, LB film thickness, found with the best fit, was fixed at 7.4 nm for Thaumatin and at 6.4 nm for Lysozyme, while the wavelength was experimentally known (0.0991 nm). Critical incident angle for Thaumatin and for Lysozyme was computed to be 0.71 deg. The delta refraction coefficients were 3.336 × 10^{-6} for glass, 2.19 × 10^{-6} for proteins. The beta absorption coefficients were about 0 for proteins, 1.68 × 10^{-4} for glass.

Curves have been fitted with a χ^2 Levenberg–Marquardt minimization procedure, which is an iterative technique commonly used for solving non linear least squares problems, with constant standard error bars of σR/R=0.005 by means of the IsGISAXS software.

**Results and Discussion**

Combination of GISAXS, synchrotron microfocus beam and computer simulation has enabled us to follow the nucleation and growth of the Lysozyme and the Thaumatin crystals.

The real GISAXS patterns are shown in Figures 2 and 3 for Thaumatin and Lysozyme, respectively.

The experimental curves of LB Thaumatin, which have been used for the fitting and simulations, are shown in Figure 4.

At 100 minutes, the particle radius of Thaumatin is about 5.62 nm, while the LB-film layer thickness is about 2.25 nm, with height ratio of 1 nm (Figure 6, where is shown the perpendicular cut along Q_z). For Figure 6, the same remarks and observations concerning Figure 5 about the excluded area are valid.

At 900 minutes from the start of the experiment, the particle radius has increased up to 40.89 nm, while on the contrary the LB-film layer thickness has decreased down to 0 nm, with a decreased height ratio of 6.30 × 10^{-2} nm. In Figure 7 the cut at Q parallel is shown at right, while at left of the same Figure 7 the cut at Q perpendicular is shown.

Previously, we hypothesized that the protein appears to transfer directly from the nano-biostructured film into the drop to directly trigger the formation of the crystal, therefore highlighting the physical interpretation of the mechanism for nanobiobtemplate-facilitated protein crystallization [35,36]. This working hypothesis however was only qualitative and not quantitative, since the GISAXS spectra were only qualitative and not quantitative, since the GISAXS spectra were only qualitative and not quantitative, since the GISAXS spectra were.

**Table 1: Modeling parameters used for the computer simulations.**

<table>
<thead>
<tr>
<th>Modeling Parameters</th>
<th>Value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Wavelength (nm)</td>
<td>0.0991</td>
</tr>
<tr>
<td>Incident angle (deg)</td>
<td>0.71</td>
</tr>
<tr>
<td>Delta – Glass (index of refraction)</td>
<td>3.336×10^{-6}</td>
</tr>
<tr>
<td>Delta – Lysozyme (index of refraction)</td>
<td>2.19×10^{-6}</td>
</tr>
<tr>
<td>Delta – Thaumatin (index of refraction)</td>
<td></td>
</tr>
<tr>
<td>Beta – Glass (absorption)</td>
<td>1.68×10^{-8}</td>
</tr>
<tr>
<td>Beta – Protein (absorption)</td>
<td>~0</td>
</tr>
<tr>
<td>LB 2 Layers thickness Thaumatin (nm)</td>
<td>7.4</td>
</tr>
<tr>
<td>LB 2 Layers thickness Lysozyme (nm)</td>
<td>6.4</td>
</tr>
</tbody>
</table>

**Five different models have been tested**

- **Model 1: Reference model**
  - Thaumatin and Lysozyme modeled as cylinders, LB film thickness found with the best fit, was fixed at 7.4 nm for Thaumatin and at 6.4 nm for Lysozyme.
  - Wavelength was experimentally known (0.0991 nm).
  - Delta refraction coefficients were 3.336 × 10^{-6} for glass, 2.19 × 10^{-6} for proteins.
  - Beta absorption coefficients were about 0 for proteins, 1.68 × 10^{-4} for glass.

- **Model 2:**
  - LB film thickness found with the best fit, was fixed at 7.4 nm for Thaumatin and at 6.4 nm for Lysozyme.
  - Wavelength was experimentally known (0.0991 nm).
  - Delta refraction coefficients were 3.336 × 10^{-6} for glass, 2.19 × 10^{-6} for proteins.
  - Beta absorption coefficients were about 0 for proteins, 1.68 × 10^{-4} for glass.

- **Model 3:**
  - LB film thickness found with the best fit, was fixed at 7.4 nm for Thaumatin and at 6.4 nm for Lysozyme.
  - Wavelength was experimentally known (0.0991 nm).
  - Delta refraction coefficients were 3.336 × 10^{-6} for glass, 2.19 × 10^{-6} for proteins.
  - Beta absorption coefficients were about 0 for proteins, 1.68 × 10^{-4} for glass.

- **Model 4:**
  - LB film thickness found with the best fit, was fixed at 7.4 nm for Thaumatin and at 6.4 nm for Lysozyme.
  - Wavelength was experimentally known (0.0991 nm).
  - Delta refraction coefficients were 3.336 × 10^{-6} for glass, 2.19 × 10^{-6} for proteins.
  - Beta absorption coefficients were about 0 for proteins, 1.68 × 10^{-4} for glass.

- **Model 5:**
  - LB film thickness found with the best fit, was fixed at 7.4 nm for Thaumatin and at 6.4 nm for Lysozyme.
  - Wavelength was experimentally known (0.0991 nm).
  - Delta refraction coefficients were 3.336 × 10^{-6} for glass, 2.19 × 10^{-6} for proteins.
  - Beta absorption coefficients were about 0 for proteins, 1.68 × 10^{-4} for glass.
were quite less optimal than the Thaumatin one due to a film was indeed possible in a different way, because the acquired data and paving the way for further research in the field.

nano-scale level, thus shedding light on protein nanocrystallography can help us in understanding the biological processes at sub-micron and complex and difficult to interpret. Indeed only computer simulation can help us in understanding the biological processes at sub-micron and nano-scale level, thus shedding light on protein nanocrystallography and paving the way for further research in the field.

For Lysozyme, a comparison between with and without LB-thin film was indeed possible in a different way, because the acquired data [34] were quite less optimal than the Thaumatin one [35,36] due to a poor alignment [34]. The experimental curves are shown in Figure 5, where at Q perpendicular cut the difference between the intensity of the scattering of the LB Lysozyme, reaching its optimal growth, and the intensity of the classical structure, suffering more from radiation damage, is strikingly visible. The process of crystal growth previously found for Thaumatin was found also for Lysozyme: in Figure 8, the Gaussian fit of the Yoneda peak region of LB-Lysozyme monitored at start and at end of the crystallization process, showing the gradual increase in R (which is the ratio of crystal protein scattering volume to glass scattering volume elevated to the square). At Q perpendicular cut, R is 0.27 at the beginning (Figure 8, left) and gradually shifts to 1.13 (Figure 8, right).

Taken together the data of Lysozyme and of Thaumatin, we have proved that LB-thin film acts a transferring nanobiotemplate and can really enhance and facilitate crystallization growth, which is often difficult and demanding.

Moreover, the semi-quantitative findings we obtained are in perfect agreement with the model hypothesized in Gebhardt et al. [35,36].

**Conclusion**

The models here introduced are based on the submicron GISAX experiments being previously carried out at the ID13 beamline at ESRF on Thaumatin [35,36] and Lysozyme [34] and point to an highly unstable time dependent growth for Lysozyme crystals contrary to what is happening for Thaumatin growth. In addition the lysozyme experimentation appear compatible with a model where the LB crystals keep growing at a constant rate while the classic crystals interrupt their growth in the same time interval.

LB-grown proteins show peculiar and unique features at the submicron size [51]. LB-assisted crystal growth was previously studied by means of AFM, *ex situ* and *in situ* μ-GISAXS [52,53] but obtained data were complex and difficult to reduce. IsGIXAS has enabled to model the crystal growth, even though with the limitations and the difficulties we underlined in the introduction section.

Our previously hypothesized model of LB-based crystal growth [35,36] was here confirmed from a semi-quantitative point of view.
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