Gd$^{3+}$-Anionic Linear Globular Dendrimer-G$_2$-C595 A Dual Novel Nanoprobe for MR Imaging and Therapeutic Agent: An In Vitro Study

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Abstract

Early cancer detection using MR imaging is of high global interest as a powerful non-invasive modality. The aim of this study was to synthesize a nano-dendrimer and its conjugate with C595 mab against breast cancer cell, followed by its chelating with Gd$^{3+}$. At the end, its ability as a nanosized probe for detection of breast cancer cells was investigated. For this reason, anti-MUC-1 mab C595 was coupled to a biocompatible anionic linear globular dendrimer G2 (ALGDG$_2$) (Poly Ethylene Glycol PEG core and citric acid shell) followed by loading with Gd$^{3+}$. MR imaging parameters of the prepared nanconjugate was investigated in vitro performing several studies such as 1H-NMR and 17O-NMR, MUC-1 antigen. The obtained data showed a powerful relaxations as well as selective MUC-1 antigen and cell binding. Findings of this study showed that Gd$^{3+}$-ALGDG2-C595 nano-probe is potentially, a selective breast molecular imaging agent.

Keywords: MR imaging; Anionic linear globular dendrimer; C595; MUC-1; Breast cancer detection

Introduction

An important method for observing of nanosized contrast agents and their delivers into the tumor is selective imaging methods such as MR imaging for better targeting cancer. The fact highly depends on the specific carrier for the cancer cells that might be distinguished with attractive agents such as monoclonal antibodies or ligands. In MR imaging, contrast agent using nanoparticle plays an important role in this modality. Because of the size of cellular or subcellular units, macromase has many obvious artifacts comparing to the nanosize in MR imaging [1-6]. For example, conventional microsize cancer contrast delivery suffers some insufficiencies of delivery, inappropriate targeting, toxicicological effects or impaired transport to cancerous site [5-8].

However, microsized cell entering carriers cannot traverse in a diffusion pattern through cells or pores including tumoric cells with pore sizes up to 380–780 nm. In confirmation, the best complex for tumor MR imaging applications would be a targeted nano-carrier complex [7,9-11]. Drug delivery using polymeric carriers is of global interest. In this regard, dendrimers (nanosized polymers) have been applied for delivering of contrast agents in MR imaging.

The biochemical properties of dendrimers, including their monodispersity, water solubility, drug loading ability and large number of functionalizable peripheral groups make these macromolecules suitable candidates for evaluation as both diagnostic and therapeutic tools. Using of safe nanocarriers such as anionic linear globular dendrimers is interesting in this regards [10-13]. Biocompatible properties of dendrimers such as log P, biodegradability, non-cytotoxicity and non-immunogenecity characteristics must be checked both under in vitro and in vivo conditions for application in MR imaging.

One generations of a highly water soluble anionic linear-globular dendrimer G2 (MW<2000 Da), (Poly Ethylene Glycol core) and citric acid periphery surface, was selected for the synthesis and subsequent MR imaging. This dendrimer has shown good capacity of drug loading in cancer therapy previously [12,13]. Monoclonal antibodies are among the best selective cancer MR imaging carrier of pharmaceuticals [14,15]. One of the targets, MUC-1, a high molecular weight transmembrane glycoprotein antigen is breast specific membrane antigen and are molecular target for a novel imaging for breast cancer [1-5].

C595 is an IgG1, a Monoclonal Antibody against human MUC [12,13]. Several studies has shown that Mab C595 is a useful antibody either alone or incorporated with other therapeutic methods to treat the human breast cancer [8,14,15].

MR imaging is a precise more sensitive and noninvasive diagnostic pattern based on differences between relaxation ratios of protons in water and provides important graphical images. Current MR imaging contrast agents such as Gd$^{3+}$-DTPA (Magnevist$^\text{®}$) improve tissue elucidation in MR images but not as well as radiopharmaceuticals which act more specifically [12,14-17].

This is the first experiment to describe synthesis and in vitro assessment of novel nanoconjugate contains ALGDG2 loaded Gd$^{3+}$ and monoclonal antibody C595 as a selective breast molecular imaging. In fact, conjugation of dendrimer to C595 and Gd$^{3+}$ loading makes a novel nanocontrast agent with potential imaging for detection of breast cancer cells.

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Materials and Methods

Preparation of the Gd\(^{3+}\)-ALGDG\(_2\)-C595 nanoconjugate

Anionic Linear Globular Dendrimer-G2 (ALGDG2) was synthesized based on literature [12,13]. Briefly, PEG-600 was chosen as the core and reacted with citric acid in the presence of excess amounts of thionyl chloride or EDC/DCC and the dialysis bag (cut off 2000 Da, Spectrum™, USA) was used for the purification. To synthesize the C595-dendrimer conjugate, 75 μmol ALGDG2 was reacted with 0.01 μmol EDC and 0.05 μmol Sulfo-NHS in 2 ml PBS or DDW for at least 5 minutes at pH=5.5-6 and the reaction allowed to reach to room temperature.

Thereafter, activated dendrimer was added dropwise to the solution containing 1 μmol C595 in 2 ml PBS medium in the presence of 1 mmole tri-ethyl-amine and the pH was adjusted to 7.5-8 and the reaction allowed continuing for 12 hrs at room temperature. To purify the conjugate, the reaction mixture was dialyzed with cut off of 10 KDa (Sigma, USA). To further purify the dialyzed solution was eluted through a Sephadex G-25 Fine* (Pharmacia-Fine Chemicals, Sweden) and the tubes containing the conjugate were selected for the next step (e.g., lyophilization, Gd\(^{3+}\) loading). All steps were monitored by Thin Layer Chromatography (TLC) method. Finally, 15 μmol GdCl\(_3\) was added to 1 μmol of conjugate at room temperature and the reaction mixture was allowed to stir at pH=7.5 for at least 2 hrs.

Afterwards, to remove excess free Gd\(^{3+}\) ions the reaction pH was increased to 9 and free Gd\(^{3+}\) ion was precipitated and filtered. To increase the purity the reaction mixture was dialyzed.

Purification

To purify dendrimer-antibody conjugate sephadex G-25 fine* (gel filtration chromatography) was used. Each external ml of eluent buffer of reaction mixture was collected separately in a numbered tube and its UV-OD at 280 nm was monitored to find antibody-dendrimer conjugate as well as nonconjugated antibody. To find dendrimer conjugated C595 monoclonal antibody TLC was performed. High Pressure Liquid Chromatography (HPLC) was also performed at small sample amounts using 10 mm×250 mm pre-packed column (at room temperature). Preparative RP-HPLC experiments were also performed using Kromasil C8, 13 μm, 100 Å silica media pre-packed in 10 mm×250 mm column (Eka Chemicals, Bohus, Sweden).

Gd\(^{3+}\)-FTIR Spectroscopy

To investigate whether or not the changes occurred after Gd\(^{3+}\) loading Fourier Transform Infrared (FTIR) spectroscopy (Thermonicolet, NEXUS 870, and Waltham, MA, USA) was employed by performance on nanoconjugate before and after Gd\(^{3+}\) loading.

Protein measurement

The assay performed in microplates based on micro Lowry assay [13-15] that has been adapted to microplates and a standard curve was prepared as following procedure. Briefly, bovine serum albumin (BSA) powder was dissolved in distilled water and diluted to a concentration of 1 μg/μl. A series of dilutions (5, 10, 20, 40, 60, 80, and 100 μg/well) were prepared and used in triplicate/100 μl. Different concentrations of protein were prepared (0-100 μg/100 μl) and a standard curve was obtained. The same procedure was performed for Gd\(^{3+}\) loaded nano conjugate and C595 alone.

Size measurement and TEM/SEM imaging

Nanosize was determined using a Brookhaven ZetaPALS (Malvern, Instrument) system for size and zeta potential distribution for both dendrimer and conjugate before and after conjugation. Beckman Multisizer Coulter equipped with a 1 nm or 100 nm apertures has been performed to depict the particle size distribution. The conjugates were also characterized by TEM (JOEL 1230; accelerating voltage, 100 kV). For TEM/SEM of samples, one drop of Gd\(^{3+}\)-ALGDG\(_2\)-C595 aqueous suspension was dispersed on copper grid and the excess volume was removed. The samples were used after drying at room temperature.

Relaxivity measurement

\(^1\)H-NMR: Water proton relaxivity ratio at different lamor frequencies (MHz) was determined by using a spinmaster spectrometer (Stelar, Mede, Italy) set at 0.5 Tesla; the inversion recovery method was used (Number of experiments 16 and 4 scans). 90°-pulse width was set 3.5 milliseconds (ms), and the reproducibility error of the T\(_1\) data was ± 0.75%. The temperature was monitored by an air-flow heater equipped with a copper-constantan thermocouple. The proton relaxivity (1/T\(_1\)) profiles were measured on a Koenig-Brown field-cycling relaxometer over a continuum of magnetic field strengths from 0.00024 to 1.2 T (corresponding to 0.0-50 MHz proton Larmor frequencies). The relaxivity measurement performed under computer monitoring with 1/T\(_1\) of ± 1.2%.

\(^{17}\)O-NMR: Variable-temperature \(^{17}\)O-NMR determinations were obtained on JEOL EX-90 (2.1 Tesla) equipments containing with a 5 mm probe. D\(_2\)O used as external lock and 2.6% \(^{17}\)O isotope solutions were used as well. The obtained transverse relaxivity ratios were calculated from signal width at 0.5 heights. More explanations were reported in supplementary materials [17,18].

In vitro cell binding and imaging: To elucidate the specific binding of C595 antibody, encountering the conjugation with Gd\(^{3+}\)-ALGD-G2, to MUC-1 over expressing cells T47D, the experiment was designed and performed. The experiment was performed on two different cancer cell lines T47D (MUC-1 over-expressed) and SKOV3 (not MUC-1 over-expressed). Before the experiments Gd\(^{3+}\)-loaded mab C595-dendrimer was conjugated covalently to a fluorescent agent red alexa fluor® 610 dyes. The cells were incubated with 20 nM of nanoconjugate for at least 60 min and thereafter cells were washed twice with PBS and the washed cells were placed under a Fluorescent Research Biological Microscopy System (BW OPTICS, China) and the images were taken from the cells at due time intervals.

Immunoreactivity: To ensure the right conjugation of dendrimer to antibody C595, antibodies detection (intact C595 and conjugated C595 to dendrimer) reactive with the MUC1 antigen was performed by ELISA considering some modifications [19,20]. Briefly, 100 μl/well of 1 μl/ml BSA was dispensed onto Falcon III PVC 96 wells plates and permitted to dry during the night at 37°C. Then the solution was washed and 50 μl containing MUC-1 core protein (100 μg/ml) and 50 μl of carbodiimide (1-cycloexil-3-[2 morpholinoethyl] carbodiimide metho-p-sulphonate (Sigma,USA) were suspended in duplicates. Then after, the wells were washed and 150 µl (blocking buffer) was exposed for 1 hour at room temperature, plates were then again washed/diluted samples (C595 and C595-conjugated dendrimer-Gd\(^{3+}\)) in blocking buffer (1:40 for IgG measurement) were performed with incubation at 4°C all over the night. After washing, 50 μl of peroxidase conjugated goat anti-human IgG in PBS Tween-BSA 0.1% were exposed and with an incubation time of 1 hour, the reaction was advanced with 50 μl aqueous solution of ABTS in 0.1 M citric-acid/0.2 M Na\(_2\)PO\(_4\) H (pH=5). Finally after 1 hour incubation in dark room, (OD) Optical Density...
was recorded at 405 nm. Based on the obtained data the comparisons were performed.

Results and Discussion

Purification and protein assay

Purification assay performed by RP-HPLC and the data shown a retention time of 7, 12 and 13 min for dendrimer, C595 alone and dendrimer-C595 conjugate, respectively with the purity of above 95% (Figure 1A). For protein assay each 100 µg nanoconjugate contained 84.3 ± 4 µg protein regarded to Mab C595 while each 100 µg intact Mab C595 contained >98 µg protein. Analytical RP-HPLC chromatogram was shown in figure 1B (The data were superimposed). As can be seen from this figure, the purity of the compounds was obtained more than 95% according to AUC, area under the curve of each peak (Figure 1).

FTIR spectroscopy

Clear changes in FTIR peaks before and after Gd³⁺ loading was occurred and this indicates the essential interaction of Gd³⁺ ions and dendrimer-C595 conjugate (Figure 2).

Gd³⁺ content and Size/TEM/SEM results

Inductively coupled plasma mass spectrometry (ICP-MS, Perkin Elmer Optima 3100XL) data showed 11.01 ± 4% (n=3) Gd³⁺ in each 100 µg nanoconjugate. Size distribution shows that dendrimer alone has an average size of 25 nm and after conjugation and gadolinium loading the average aggregation size reached to 61 nm. The apparent view of nanoparticles was also shown in SEM and TEM images. Figures 3A-3D shows TEM illustration of dendrimer, Gd-dendrimer-C595, Gd-dendrimer-C595 (SEM) and size distribution of dendrimer before and after Gd³⁺ and C595 bioconjugation. The TEM picture of Gd-dendrimer-C595 showed high average more than 2 nm (Figure 3).

Relaxivity studies

The relaxivity data were illustrated in figures 4 and 5. As it can be found gadolinium loaded nanoconjugate showed an extreme temperature, concentration and frequency intendancy. Increase in the temperature, concentration or frequency increased the paramagnetic potential of the nano-probe. Because of low dose, the conjugate showed a less paramagnetic activity than that of standard agent like Magnevist® but, it is interesting that by increasing the temperature, concentration and frequency the relaxivity is increased similar to Magnevist® at high concentration. Both (figures 4 and 5) showed that nanosize contrast agent produced enough relaxivity (1H-NMRD and 17O-NMR profiles) for breast cancer cells and the results showed its higher relaxivity in comparison with Magnevist®.
Proton Lamor relaxivity at different doses of nanoconjugate and formation as well as Gd\(^{3+}\) loading. The negative charge of dendrimer G2 [16,18-22]. Based on the obtained observations here, C595 suffers an inactivation and this is observed sometimes occasionally occur while one or both biomolecules active site (covering kinetic) not producing any biological activity complications. The complications regarding to its citric acid shell which raise potent Gd\(^{3+}\) complex nanoprobe in comparison with unbound C595 (Figure 6A and B).

The interesting capability of anionic linear dendrimer G2 is regarding to its citric acid shell which raise potent Gd\(^{3+}\) complex formation as well as Gd\(^{3+}\) loading. The negative charge of dendrimer G2 protect nanoprobe from any surface-surface toxic interactions between the normal cell body and the conjugate.

One of the main criteria of biomolecular conjugation is regarding to not producing any biological activity complications. The complications occur while one or both biomolecules active site (covering kinetic) suffers an inactivation and this is observed sometimes occasionally [16,18-22]. Based on the obtained \textit{in vitro} observations here, C595 anti-MUC-1 serves its activity after dendrimer conjugation and this fact leads to next nano-conjugate \textit{in vivo} success. In confirmation, there are some reports on the anticancer activity of unbound C595 which suggests anticancer effects for C595 [20-22].

**Cell binding and immunoreactivity assay**

As indicated in (figure 6), fluorescent images obtained from treated SKOV3 and T47D cells with 20 nm. Images were taken after cell wash. Immunoreactivity assay showed also no alteration MUC-1-Gd-dendrimer-C595 interaction diactivity comparison with C595. Interesting results were obtained while Gd\(^{3+}\)-ALGDG2-C595 did not bind to SKOV3 cells but a good T47D cell binding were recorded after 60 min exposure to MUC-1 receptor expressed cells. This fact confirms characteristics of MR imaging nano-generated molecular probe. In other word, specific MUC-1 binding and specific activity of nanoprobe and also dendrimer conjugation with Gd\(^{3+}\) loading to C595 mab did not produce any dynamic complications. Immunoreactivity assay also showed a good MUC-1 reactivity between Gd-dendrimer-C595 did not produce any dynamic complications. Immunoreactivity assay showed also no altered MUC-1-Gd-dendrimer-C595 interaction diactivity comparison with C595.

The present study shows a successful strategy in generating a powerful nanosize probe considering the biocompatibility and appropriate Gd\(^{3+}\) loading capability to find and detect breast cancer cells. The capability of nanosize contrast agent to produce enough relaxivity (\(^{1}H\)-NMRD and \(^{17}O\)-NMR profiles) and specific binding characteristics of MR imaging nano-generated molecular probe. In other word, specific MUC-1 binding and specific activity of nanoprobe and also dendrimer conjugation with Gd\(^{3+}\) loading to C595 mab did not produce any dynamic complications. Immunoreactivity assay also showed a good MUC-1 reactivity between Gd-dendrimer-C595 nanoprobe in comparison with unbound C595 (Figure 6A and B).

**Comparative Immunoreactivity Assay**

![Comparative Immunoreactivity Assay](image)

**References**


