In vivo Efficacy of PAMAM-Dendrimer-Cisplatin Complexes in SKOV-3 Xenografted Balb/C Nude Mice

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Abstract

Loco-regional delivery of cisplatin by Intraperitoneal (IP) administration in ovarian cancer is highly advantageous, since it exposes high concentrations of cisplatin to tumors in the peritoneal cavity. PAMAM-dendrimer-cisplatin complexes are expected to enhance the penetration of tumors in the peritoneal cavity, and aid in enhancing antitumor efficacy of cisplatin. In the present study, PAMAM G4 NH2 and Biotin PAMAM G4 NH2 dendrimer cisplatin complexes were administered intraperitoneally to SKOV xenografted athymic nude mice at a dose of 4 mg/kg. The increase in lifespan of tumor bearing mice and biodistribution of cisplatin in various organs was evaluated after IP administration of cisplatin and dendrimer-cisplatin complexes. The lifespan of mice increased by 41.93% and 25.8%, after treatment with PAMAM G4 NH2 and Biotin PAMAM G4 NH2 dendrimer cisplatin complexes, respectively. A 3-fold increase in the levels of platinum in plasma was observed, after administration of both PAMAM G4 NH2 and Biotin PAMAM G4 NH2 dendrimer cisplatin complexes. Biodistribution studies have shown higher accumulation of platinum in liver, spleen and kidneys with PAMAM G4 NH2 dendrimer-cisplatin complexes. The increased plasma concentration and enhanced tissue accumulation after IP administration of dendrimer-cisplatin complexes offer advantage of administering low dose of cisplatin, which would reduce the dose-dependent toxic effects of cisplatin.

Keywords: Cisplatin; PAMAM; Biotinylated dendrimer-cisplatin

Introduction

In the United States, ovarian cancer ranks ninth among most common cancers and ranks fifth in cancer deaths, among women. It is estimated that approximately 22,280 women will be diagnosed and 15,500 women will die from ovarian cancer in 2012 [1]. It is also estimated that ovarian cancer will occur in 190,000 women and causes death in 114,000 patients annually worldwide [2]. According to the American Cancer Society, the rate at which women are diagnosed with ovarian cancer has been reduced in the past 20 years. However, the 5-year survival rate is still dismal at 46%. It was also reported that if ovarian cancer was detected and treated before it metastasizes; the 5-year survival rate will be around 93%. Unfortunately, less than 20% of all ovarian cancers are detected at this early stage [3]. The first-line treatment of ovarian cancer involves use of platinum based chemotherapeutic agents, such as cisplatin along with other anti-cancer drugs such as paclitaxel [4-6]. Cisplatin is widely used for the treatment of peritoneal carcinomatosis by Intraperitoneal (IP) administration [7,8]. Although clinical studies have demonstrated the superior efficacy of IP chemotherapy of cisplatin compared to Intravenous (IV) chemotherapy, IP cisplatin chemotherapy suffers from major drawbacks, such as poor penetration of cisplatin into peritoneal tumors and dose-limiting systemic toxicity due to infiltration of cisplatin into systemic circulation through peritoneum.

The first report on the potential of Intraperitoneal (IP) administration in ovarian cancer was published by Dedrick et al. [9], in Cancer Treatment Reports. A theoretical modeling study supporting the examination of IP antineoplastic drug delivery for ovarian cancer was presented, and suggested that tumors in the peritoneal cavity should be exposed to higher cytotoxic drug concentrations with regional IP treatment [9]. Because of its low molecular weight and water solubility, cisplatin was reported to enter the systemic circulation rapidly after IP injection, leading to low concentrations in the peritoneal cavity and increasing risk of systemic toxicity [10]. The other limitation is that IP chemotherapy of cisplatin is limited to patients whose residual tumor nodules are less than 0.5 cm after a surgical debulking [11]. Poor penetration of cisplatin into the inner core within large tumor masses is also a reason for failure of IP chemotherapy of cisplatin [12]. To improve cisplatin penetration, either cisplatin should be in contact with the tumor for a longer period of time, or should be administered at very high concentrations. Both of these strategies have very high propensity of resulting in systemic side effects such as nephrotoxicity and myelotoxicity [13]. One attractive strategy to improve drug delivery to the peritoneal cavity and to reduce toxicity is use of tumor targeted drug delivery systems.

We have previously reported the potential of biotinylated PAMAM dendrimers as targeted drug delivery systems for cisplatin to ovarian cancer [14,15]. Biotinylated dendrimer-cisplatin complexes were shown to be taken up avidly by ovarian cancer cells because of great appetite of cancer cells for vitamins like biotin [16]. So far biotinylated dendrimer-cisplatin complexes were not evaluated for IP chemotherapy. Herein we report the in vivo biodistribution of dendrimer-cisplatin complexes prepared using simple PAMAMG4 and biotinylated PAMAM dendrimers, and their efficacy in prolonging the life span in a clinically relevant SKOV-3 xenografted murine ovarian cancer model.

Materials and Methods

Materials

PAMAM dendrimers (G4 NH2) were purchased from Dendritic Nanotechnologies Inc., (Mount Pleasant, MI, USA). Cisplatin, 3-[4, 5-dimethylthiazol-2-yl]-2, 5-diphenyl tetrazolium bromide (MTT),
2,5 Dihydroxybenzoic acid (DHB), trifluoroacetic acid, nickel chloride (NiCl₂) and insulin (recombinant human) were purchased from Sigma-Aldrich (St. Louis, MO, USA). Biotinylating reagents Sulfo-NHS-LC-Biotin (Mr 556), Morpholinouethane Sulfonic acid-(MES) buffered saline packs were purchased from Fluka Chemicals, (Steinheim, Switzerland). Dialysis membranes were purchased from Spectrum Laboratories (Rancho Dominguez, CA, USA). Omni Trace® nitric acid was purchased from EMD Biosciences (Gibbstown, New Jersey, USA). The Plasma Cal tune A, tune B, platinum standard (1000 μg/mL) and iridium standard (1000 μg/mL) were purchased from SCP Science (Baie D’Urfé, Quebec, Canada).

Synthesis and characterization of biotinylated PAMAM dendrimers

Biotin-conjugated PAMAM dendrimers were prepared, as reported previously [15,17]. PAMAM G₄ NH₂ dendrimers (10 mg/mL) dissolved in phosphate buffer pH 9.0 were added to sulfo-NHS-LC-biotin at 1:30 molar ratio, and stirred for 2 h at room temperature. The unconjugated biotin was separated by dialyzing reaction mixture against deionized water and lyophilized (Free zone 2.5, Labconco Corporation, Kansas City, MO, USA), to yield a white product. The final product was characterized for attachment of biotin by proton nuclear magnetic resonance (1H NMR, Bruker AMX-400 spectrometer, Bruker, Rheinstetten, Germany), using D₂O as solvent at a concentration of 5 mg/mL. Degree of biotinylation was calculated using Bruker MALDI-TOF (matrix assisted laser desorption/ionization-time-of flight) using 2, 5 dihydroxybenzoic acid in 0.1 M trifluoroacetic acid as the matrix [15].

Preparation of dendrimer-cisplatin complexes

Dendrimer-cisplatin complexes were prepared by using a method developed in our lab previously [14]. Briefly, cisplatin was completely dissolved in 7.5 mL of water at 2 mg/mL concentration in a round bottomed flask. To this solution 20 mg of biotinylated and unconjugated dendrimers were added dropwise under stirring. The mixture was reacted for 4 hrs and dialyzed (3.5 kDa MW cutoff) against deionized water for 24 hrs. The final reaction product was lyophilized (Free zone 2.5. Labconco Corporation, Kansas City, MO, USA), to yield a white product. Drug loading efficiency of dendrimer-cisplatin complexes was determined using inductively couple plasma-mass spectroscopy (ICP-MS). Briefly, 1 mg of dendrimer-cisplatin complex was dissolved in 1 mL of 0.9% NaCl solution. 100 μL of this solution was aliquoted and added to 5 mL of 1% HNO₃ with 10 ng/mL iridium as the internal standard.

Quantification of cisplatin by ICP-MS

The ICP-MS system was comprised of an X Series ICP-MS (Thermo Electron Corporation, Madison, WI, USA) equipped with a Cetac 500 auto sampler (Cetac Technologies, Omaha, NB, USA). Analysis was performed in X-series default mode using 2.Xi+screen. The results were analyzed using PlasmaLab software (Thermo Electron Corporation). Major isotopes of platinum and iridium were monitored at m/z 195 and 193, respectively. Sample 6 nebulization was performed using a concentric nebulizer and detection modes for both isotopes were “scanning”. Details of ICP-MS operating conditions are given in table 1. Quantification was based on the mean (n=3) intensity ratios for platinum and iridium against a calibration curve using linear regression analysis. All standards and samples were prepared in 1% OmniTrace® nitric acid. A standard platinum calibration curve was prepared with concentrations from 0.1 to 1000 ng/mL. In all standard solutions iridium was added to get a final concentration of 10 ng/mL.

Sample preparation for biodistribution studies

Plasma (100 μL) was separated from freshly collected blood (200 μL) by centrifugation at 4000 rpm. Plasma samples were digested with concentrated nitric acid (HNO₃) (70%) and after digestion samples were dried at 85°C overnight. Similarly, isolated tissues were homogenized using an Omni 2000 Tissue Homogenizer, Omni international, GA, USA, and were digested with concentrated HNO₃ (70%) and dried at 85°C overnight. Both plasma and tissue dried samples were reconstituted with 1% HNO₃ and 10 ng/mL of iridium was added as internal standard prior to analysis by ICP-MS. The standard graph of cisplatin was prepared by spiking cisplatin with blank plasma and tissues using concentrations, ranging from 0.1 ng/mL to 1000 ng/mL.

In vivo anti-tumor efficacy of dendrimer-cisplatin complexes

Animals: Female athymic nude mice 4 weeks old were procured from Harlan Laboratories (Indianapolis, IN, USA) and were housed at Pharmaceutical Research Facility, Texas A&M Health Science Center, Kingsville, Texas. All mice were housed and maintained under specific pathogen-free conditions according to guidelines of the American Association for Accreditation of Laboratory Animal Care (AAALAC), and the facility was operated in accordance with current regulations and standards of the U.S. Department of Agriculture (USDA), U.S. Department of Health and Human Services, and NIH. All protocols were approved by the institutional animal care and use committee of the College of Pharmacy (Protocol No. 10039). The mice were maintained on a standardized 12-h light and 12-h dark cycle and were provided access to food and water ad libitum. Animals were fed with irradiated 5053 PicoLab® rodent diet 20, PMI Nutrition International, St. Louis, MO, USA.

SKOV xenografted murine ovarian cancer model

SKOV tumor model was chosen because SKOV cells have the ability to get implanted directly on the peritoneal wall, resulting in numerous visible microtumor nodules and parietal thickening, resembling disease in humans [18]. Tumors were initiated by IP injection of SKOV cells (5x10⁶), and mice were separated into four groups of 8 mice each for survival studies and three groups of 10 mice each for biodistribution studies. Tumors established by IP injection of cells reflect the growth

<table>
<thead>
<tr>
<th>Flow Conditions (L min⁻¹)</th>
<th>Torch alignment (mm)</th>
<th>Ion optics (volts)</th>
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<tbody>
<tr>
<td>Plasma flow 18.0</td>
<td>Sampling depth 130</td>
<td>Lens 1 0.28</td>
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<tr>
<td>Auxiliary flow 0.90</td>
<td>Lens 2 -29.02</td>
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<tr>
<td>Sheath gas 0.25</td>
<td>Lens 3 -195.29</td>
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<tr>
<td>Nebulizer flow 0.95</td>
<td>Pole Bias 0.51</td>
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<td></td>
<td>Hexapole Bias -3.02</td>
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<td></td>
<td>Extraction -235.29</td>
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Table 1: ICP-MS instrument settings.
pattern of advanced epithelial ovarian cancer and is widely used as a clinically relevant model for studying epithelial ovarian cancer [19]. Mice were evaluated weekly for tumor growth and/or ascites fluid accumulation. The animals were considered to have developed ascites if they showed clinical signs of tumor formation such as reduced movement, slightly hunched back, matted fur and reduction in animal weight. All animals in survival studies were sacrificed by 50 days after tumor initiation.

Treatment protocol

Cisplatin, PAMAM G4 NH2, cisplatin and Biotin-PAMAM G4 NH2, cisplatin, were administered by IP injection (500 μL) with PBS as the vehicle. The control groups of animals were administered PBS and other groups received 4 mg/kg equivalent of cisplatin either in solution or as dendrimer-cisplatin complexes four times with an interval of a week between each administration. Animals were euthanized using CO2 at 4 hrs and 24 hrs and blood was collected by cardiac puncture. In the biodistribution study brain, lung, heart, liver, kidney, and spleen, were isolated.

Statistical analysis

Statistical analyses were performed by Graph Pad Prism 5.0 and evaluated for statistically significant differences by one-way ANOVA and F<0.05 was considered statistically significant. Percentage of reaction medium was performed using two different solvents 0.9% sodium chloride and deionized water. The loading efficiency was very low (~0.1-2%), when 0.9% sodium chloride was used as reaction medium. However, the loading efficiency increased to ~10-11% when deionized was used as reaction medium. The high chloride ion concentration in 0.9% sodium chloride which inhibits the hydrolysis (aquation) of cisplatin and henceforth its reactivity, with dendrimers might be the reason for low loading. Our data corroborates with recent report by Kirkpatrick et al. [20], which showed that improved hydrolysis (aquation) of cisplatin using silver nitrate resulted in improved loading of cisplatin to dendrimers. The advantage of our dendrimer based nanocarrier system is evident as our loading efficiency is significantly higher than other nanocarrier formulations of cisplatin such as Lipoplatin™ (8.9%) (a liposomal cisplatin formulation) [21], and PLGA-mPEG cisplatin nanoparticles (1.99%) [22].

Preparation of biotinylated dendrimer-cisplatin complexes

The drug loading efficiency of cisplatin as determined by ICP-MS was 102.9 μg per 1 mg of dendrimer (10.29%). The optimization of reaction medium was performed using two different solvents 0.9% sodium chloride and deionized water. The loading efficiency was very low (~0.1-2%), when 0.9% sodium chloride was used as reaction medium. However, the loading efficiency increased to ~10-11% when deionized was used as reaction medium. The high chloride ion concentration in 0.9% sodium chloride which inhibits the hydrolysis (aquation) of cisplatin and henceforth its reactivity, with dendrimers might be the reason for low loading. Our data corroborates with recent report by Kirkpatrick et al. [20], which showed that improved hydrolysis (aquation) of cisplatin using silver nitrate resulted in improved loading of cisplatin to dendrimers. The advantage of our dendrimer based nanocarrier system is evident as our loading efficiency is significantly higher than other nanocarrier formulations of cisplatin such as Lipoplatin™ (8.9%) (a liposomal cisplatin formulation) [21], and PLGA-mPEG cisplatin nanoparticles (1.99%) [22].

Optimization of suitable analytical method for estimation of cisplatin

Various analytical methods for cisplatin quantification in plasma and tissues were developed using UV, HPLC and ICP-MS. The suitable analytical method was chosen based on parameters such as ease of sample preparation, robustness and sensitivity. Data showed that UV and HPLC methods were not sensitive (LLOQ 1 μg/mL). Moreover, derivatization of cisplatin by DDTC in those methods made the method cumbersome. Both UV and HPLC methods were not robust...
as the results were inconsistent when pH of the sample matrix was changed. Based on these observations ICP-MS was chosen as suitable method for estimation of platinum in plasma and tissues, as it is very sensitive (LLOQ 0.1 ng/mL), robust and convenient.

**In vivo anti-tumor efficacy of dendrimer-cisplatin complexes**

PAMAM G4 NH2 and Biotin PAMAM G4 NH2 dendrimer-cisplatin complexes were investigated for *in vivo* anti-tumor efficacy by evaluating their ability to prolong survival of tumor bearing mice. Procedures involving SKOV xenograft mouse tumor model were conducted in conformity with guidelines of the American Association for Accreditation of Laboratory Animal Care (AAALAC). Mice were monitored daily for body weight and signs of tumor progression such as abdominal distension, hunched back and matted fur. For survival studies, animals were sacrificed after reaching a predetermined endpoint characterized by weight loss exceeding 15% associated with anorexia, and/or diarrhea. Survival curves for the control and the treatment groups are shown in figure 3. All survival curves for treatment groups were significantly different from the control groups (p<0.033), which were associated with median survival times of 28.5 to 32.5 days (Table 2). Treatment with IP PAMAM G4 NH2-cisplatin and Biotin PAMAM G4 NH2-cisplatin resulted in a 41.9 % and 25.8 % increase in lifespan, when compared with treatment of cisplatin alone. Moreover, treatment with IP PAMAM G4 NH2- and Biotin PAMAM G4 NH2-dendrimer-cisplatin did not reduce the body weight in comparison with cisplatin (data not shown). Survival studies clearly indicate that eventhough biotinylation enhances the targeting ability of PAMAM dendrimers, it is limiting the cytotoxic efficacy of platinum probably by interfering with their interaction with DNA in cancer cells.

**Biodistribution studies**

The platinum concentration in the plasma and tissues was determined by ICP-MS. The calibration curve was linear in the concentration range from 0.1 ng/mL to 1000 ng/mL ($R^2=0.999$), with a limit of detection of 0.05 ng/mL and limit of quantification of 0.1 ng/mL (5% standard deviation). Quality control samples, 0.1 ng/mL, 1 ng/mL and 10 ng/mL were used for method validation for accuracy and precision and the percentage coefficient of variation was <5% for all the data. The platinum recovery from cisplatin spiked tissues was plasma-93.4 ± 3.5% (mean ± SD); liver-84.5 ± 2.3 %; lungs-90.2 ± 1.2 %; heart-96.2 ± 5.3 %; kidneys - 97.9 ± 4.3 %; spleen - 96.8 ± 2.6 %; ascites-95.7 ± 5.2 %.

The biodistribution data showed that the biotin-G4 NH2 dendrimer-cisplatin complexes accumulated in significantly high concentrations in liver, heart, spleen, kidneys when compared with cisplatin alone, the results were not as good as expected, possibly because of excessive adherence of dendrimers to the peritoneal cavity wall, probably mediated by surface charge. The smaller size and surface charge of the dendrimers, which are the cardinal aspects for enhancing tumor penetrating ability, might have led to increased diffusion of cisplatin through the peritoneum into systemic circulation. As shown in figure 5, dendrimer-cisplatin complexes accumulated in significantly high concentrations in liver, heart, spleen, kidneys when compared with PAMAM G4 NH2 cisplatin and cisplatin only, with no increase in accumulation in lungs, brain and ascites. Our data corroborates with a report by Malik et al. who reported that PAMAM NH2 dendrimers of generation 4 showed high accumulation in liver [23]. As shown in figure 4, there was a 2.5 fold and 0.6 fold increased accumulation of platinum in in liver with biotin-G4 NH2- and G4 NH2-dendrimer-cisplatin complexes respectively, when compared with cisplatin alone. Liver and spleen, which are the organs of the mononuclear phagocytic system, have been shown to have a greater tendency to accumulate nanoparticulate formulations including dendrimers [24]. Moreover, IP administration of dendrimer-cisplatin complexes might have resulted in increased penetration of cisplatin through peritoneum and resulted in higher accumulation in various organs. Although a statistically significant increase in cisplatin accumulation in ascites was observed with dendrimer-cisplatin complexes as compared to cisplatin alone, the results were not as good as expected, possibly because of excessive adherence of dendrimers to the peritoneal cavity wall, probably mediated by surface charge. The smaller size and surface charge of the dendrimers, which are the cardinal aspects for enhancing tumor penetrating ability, might have led to increased diffusion of cisplatin through the peritoneum into systemic circulation. As shown in figure 5,
plasma concentrations of platinum after 4 hr and 24 hr were also higher with IP administration of dendrimer-cisplatin complexes as compared to cisplatin alone. Overall, the pharmacokinetics of cisplatin was altered after IP administration of dendrimer-cisplatin complexes.

**Conclusion**

In conclusion, all the dendrimer-cisplatin complexes studied have shown greater anti-tumor efficacy *in vivo* as compared to cisplatin alone. Though toxicity experiments were not performed in the present study, higher accumulation of cisplatin in liver and kidney suggests the need to improve the retention of dendrimer-cisplatin complexes in the peritoneal cavity, may be by using external stimuli (such as magnetic field, ultrasound, etc.) responsive nanoparticles of cisplatin. Under the control of such external stimulus, these nanoparticles may retain in the “tumor sanctuaries” interspersed across the peritoneum for extended duration and show high therapeutic activity with minimal non-target distribution and lower magnitude of side effects.

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**References**
