

Spiral Fracture of Long Bones in an Infant: Clinical and Biomechanical Challenges

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The risk of a fracture from non-accidental injury is highest in the infant age group. The incidence of fractures in children increases with age [1], so infants have the lowest overall numbers of fractures. They are also most vulnerable to child abuse as they are entirely dependent on their carers, have a limited mobility and are completely defenceless. The incidence of a fracture from non-accidental injury in children under 18 months is estimated to be 4/10 000/ year [2]. It is also estimated that in children under the age of 1 year, 25% to 50% of all fractures are due to non-accidental injury, with 40% to 80% of long bone fractures resulting from non-accidental injury [3]. Infants under 4 months with fracture are more likely to have been abused [4].

A spiral fracture of long bones of children was thought to be highly associated with non-accidental injury, but it is now recognised that it can equally occur from innocent injuries. However, literature is unclear about the significance of a spiral fracture of long bones of the very young infant. A common mechanism of an innocuous injury for this fracture is the child tripping over while running. However, an infant has very restricted mobility and this mechanism is unlikely to easily occur in the very young infant who is still non-ambulant. One study found spiral fracture pattern to be the most common abusive femoral fracture in children under 15 months [5] and no difference in the distribution of spiral fractures of femur from accidental and non-accidental injuries in children over 15 months [5]. Similarly, a systematic review indicates that spiral fracture pattern is the most common type of humeral fracture from non-accidental injury in children less than 15 months. However, this might be just because spiral and oblique fractures are more common in children under 15 months [6,7].

In the infant, clinical judgement on a non-accidental injury as the source of a spiral fracture of long bone is very difficult and clouded by the occurrence of stress fracture e.g. toddler's fracture in children, a broad spectrum of medical conditions that affect bone strength e.g. osteogenesis imperfecta, osteopenia of immaturity and rickets, and undiagnosed fractures from birth related trauma. The spiral fractures of femur are one of the common birth-related fractures, with an estimated incidence of 0.13 per 1000 live births [8]. These fractures are quite commonly unnoticed immediately post-partum as it difficult to associate features of pain with an underlying fractures in a newly born. A fracture is only suspected from unusual behavior, muscle tone, and lack of normal use of the limb. As a result, there is a delay in diagnosis of birth-related fractures in the majority of children. One study found a time delay of between 2-21 days in identifying post-partum femoral fractures [9]. This delay in diagnosis can lead to wrongfully suspecting child maltreatment [8].

A spiral fracture occurs when torsional (i.e. rotational) forces applied to the bone. A torsional force acts to twist the bone about its longitudinal axis. The narrowest region of the bone is most susceptible to a spiral fracture, as it is the least stiff section of the bone and usually experiences the highest stresses. This is why spiral fractures in the tibia commonly occur in the narrow distal third [10]. In experimental studies the average angle of the spiral fracture to the longitudinal axis of the bone is found to be between 30° and 40° [11,12]. This is in a good agreement with theoretically calculated angle of 45°, which is the plane

of maximum tension under torsional force along which the fracture line propagates. However, in clinical experience, the spiral fracture angle can vary considerably from anywhere between 20° to 90° [13]. This difference between the experimental and clinical findings is due to bone anisotropy, moments caused by simultaneous contraction of muscles attached to the bone and bony appendages that distort fracture progression [14,15]. An *in vivo* torsional injury is also associated with a bending moment that prevents endless propagation spiral fracture line.

Biomechanical research utilising human tissues and animal models is continually improving our understanding of injury mechanism and thresholds for spiral fracture. However, our overall understanding of torsion strength properties of pediatric bones is much less than that of adults' bones. From a biomechanical point of view, a structure's strength under tensional load i.e. tensional strength is related to its material properties and its cross-sectional properties, but not to its length [16-18]. However, in children the cross-section of the bone is a function of its length; therefore as paediatric bones get longer, there is compensatory increase in cross-sectional diameter to maintain strength [19]. This has implications for animal bone models used to investigate characteristics of paediatric long bone fracture. The immature animal bone model must have suitable composition and dimensions to the equivalent long bones in a particular paediatric age group. Such a model could be used to estimate bone strength under a specific loading mode e.g. torsional loading. The restrictions in matching an animal bone model to paediatric bones means that transferable biomechanical data on threshold for fractures in children is scarce. Therefore, whilst there is a widely accepted requirement for objective, science-based injury assessment tools at presents the paucity of biomechanical data prevents correlation between the mechanics and a pediatric injury criterion. A greater understanding and acceptance of biomechanical models would improve clinical understanding of the underlying cause of fracture in a child.

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