

was introduced to the polymeric solution under intensive stirring. Final mixture was filled into the polypropylene cylindrical mold and UV-irradiated for 1h at 50°C in a closed glass box. In a further step, prepared material was swollen to the equilibrium in the cation-saturated solution of Fe_2SO_4 (306 g/L) or $\text{Fe}_2(\text{SO}_4)_3 \times 7\text{H}_2\text{O}$ (213 g/L) and the alginate chains were crosslinked.

Alginate/acrylamide hydrogels synthesis by simultaneous method

The water solution of acrylamide and alginate was prepared with a fixed ratio of monomers 8:1 respectively, the water content was fixed at 86 wt%. At first, ammonium per sulfate (1 wt% by acrylamide) and MBAA (0.0006 or 0.0012 MBAA/AAM) was added to the monomer solution. The solution was stirred under nitrogen bubbling for 10 min and then degassed at $T=2^\circ\text{C}$. In a further step, CaSO_4 or $\text{CaCl}_2/\text{Na}_2\text{SO}_4$ (from 9.17×10^{-5} to 3.45×10^{-4} moles) and TMEDA (0.0025 wt%) were introduced to the solution under intensive stirring. Final mixture was filled into the PP mold and UV-irradiated for 1h at 50°C in a closed glass box.

Compression test

Elastic modules of hydrogels were obtained from compression test. According to rubber elasticity theory under the assumption of affine network model, the Young's modulus can be determined from the slope of linear dependence:

$$\sigma = \frac{f}{S_0} = Ee$$

where σ is the applied stress in Pa/m², f is the value of measured force, S_0 is the cross section of the unstrained swollen sample and e is the relative deformation of the sample. The structural parameters of the polymer network were also determined from the compressive test. The apparent crosslinking density (n_e) was determined from elastic modulus and swelling ratio data using the following equation [16]:

$$\sigma = RT \left(\frac{\Phi_{p0}}{\Phi_p} \right)^{\frac{2}{3}} \Phi_p n_e e$$

where, Φ_{p0} and Φ_p are the polymer volume fractions in anhydrous and swollen state respectively.

Swelling properties of IPN

The samples were weighed (W_d), and then swollen in distilled water for 24 h at 37°C before being weighed in a swollen state (W_s). The equilibrium water content (EWC) was evaluated as follows:

$$EWC = \frac{W_s - W_d}{W_s} * 100\%$$

FTIR spectroscopy

The FTIR spectra were performed on Bruker IFS66 spectrometer (Global source, 32 scans, DTGS detector, resolution 2 cm⁻¹) in transmission mode on KBr pellets prepared with ≈ 2 wt% of powdered dry hydrogel or solid residue.

Results and Discussion

Hydrogels preparation

Several series of hydrogels were synthesized according to the formulations presented in the Table 1. Different procedures

N°	mode	MBAA/AAM $\times 10^2$	Alginate	Cation (source; 2 mol/L)	[Cation], mol.
1 - 4	sequential	0.76; 2.27; 3.85; 5.26	Alg1	$\text{Fe}^{2+}, \text{FeSO}_4 \times 7\text{H}_2\text{O}$	---
5 - 8	sequential	0.76; 2.27; 3.85; 5.26	Alg1	$\text{Fe}^{3+}, \text{Fe}_2(\text{SO}_4)_3 \times x\text{H}_2\text{O}$	---
9 - 12	sequential	0.76; 2.27; 3.85; 5.26	Alg2	$\text{Fe}^{2+}, \text{FeSO}_4 \times 7\text{H}_2\text{O}$	---
13 - 16	sequential	0.76; 2.27; 3.85; 5.26	Alg2	$\text{Fe}^{3+}, \text{Fe}_2(\text{SO}_4)_3 \times x\text{H}_2\text{O}$	---
17 - 21	simultaneous	0.06	Alg1	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	0.92; 1.38; 2.07; 2.76; 3.45
22 - 26	simultaneous	0.06	Alg1	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	0.92; 1.38; 2.07; 2.76; 3.45
27 - 31	simultaneous	0.12	Alg1	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	0.92; 1.38; 2.07; 2.76; 3.45
32 - 37	simultaneous	0.12	Alg1	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	0.92; 1.38; 2.07; 2.76; 3.45

Table 1: Synthesized IPN hydrogels.

(simultaneous or sequential) and alginate compositions (alginate1 or alginate2) were used with variation of covalent crosslinker concentration (MBAA/AAM) and cation nature ($\text{Ca}^{2+}/\text{Fe}^{2+}/\text{Fe}^{3+}$). Two different sources of Ca^{2+} ions were used for alginate crosslinking through simultaneous procedure. It was noticed that the hydrogels containing more than 2.762×10^{-4} moles of CaSO_4 became turbid due to the low solubility of calcium sulfate in the water (0.021 g/L). To overcome this issue, CaCl_2 solution was used as a source of Ca^{2+} ions and transparent hydrogels were obtained. However, due to the perfect solubility in the water and high dissociation rate of calcium chloride, the crosslinking rate of alginate chains by Ca^{2+} ions considerably increases. As a result at high concentration of CaCl_2 solution (e.g., 811 g/L), the formation of uniform and transparent material in such conditions seems to be impossible [17]. Instantaneous gelation leads to quasi-spontaneous crosslinking of the alginate chains slowing their diffusion in the volume, inducing high and low crosslinked zones. The presence of such an inhomogeneity during the radical polymerization and crosslinking of the acrylamide creates obstructions for propagation of the network and distribution of the crosslinks. Therefore, other routes achieving uniform gel structure are proposed such as the preparation with the use of CaCO_3/d -glucono- δ -lactone (GDL) system, a source of ions with low dissociation rate which could increase with the pH [18]. Thanks to the gradual dissociation of carbonate and the consecutive slow crosslinking rate of alginate, homogeneous hydrogel could be prepared. However, due to the presence of carbonate particles, final materials are not transparent. As alternative way of reducing the crosslinking rate of the alginate, we applied the redox system of $\text{CaCl}_2/\text{Na}_2\text{SO}_4$. Comparing with the CaCl_2 solution, the dissociation rate of chosen redox system is lower due to the simultaneous ionic-exchange reaction. IPN hydrogels were also prepared by two-step polymerization procedure. This process includes the following successive stages: the synthesis of acrylamide network in the presence of sodium alginate chains leading to the formation of the semi-IPN structure and the further swelling in ion-saturated water solution leading to the crosslinking of alginate chains and the formation of full-IPN structure.

Hydrogels characterization

After the synthesis, all the interpenetrating polymer networks as well as the pure sodium-alginate, poly(acrylamide) (pAAM) and

alginate beads crosslinked with $\text{Ca}^{2+}/\text{Fe}^{2+}/\text{Fe}^{3+}$ ions were analyzed thanks to the FTIR spectroscopy. As expected, the FTIR spectrum of pAAm exhibits the bands of NOH (stretching, $3400\text{-}3200\text{ cm}^{-1}$), C=O (stretching, 1670 cm^{-1}), NH (bending, 1622 cm^{-1}), CH (stretching, 2932 cm^{-1}) and CH (bending, $1500\text{-}1300\text{ cm}^{-1}$). In the case of the spectrum of pure NaAlg, different peaks were observed: broad one assigned to the vibration of -OH group at 3445 cm^{-1} , peaks at 1612 and 1421 cm^{-1} corresponding to the asymmetric and symmetric stretching vibrations of -COO⁻ group, peak at 1050 cm^{-1} assigned to C-O group, the signal of Na-O appears at 820 cm^{-1} [19]. Spectra of the different sodium alginates were similar. However, comparison of the NaAlg spectrum and the spectrum of alginate crosslinked either by Ca^{2+} , Fe^{2+} or Fe^{3+} shows significant shifts of the -COO⁻ group and metal-O bands to the higher values (Table 2) giving evidence of its chelation. Those shifted values depend on the metal-carboxylate coordination type [20].

Chelation of two parallel alginate chains with divalent metallic ions leads to a planar geometry configuration, so-called "egg box", while chelation with trivalent metallic ions induces alginate complex with the coordination type $(\text{COO})_3\text{M}$ resulting in a non-planar geometry [14,21]. Such a tridimensional bonding model leads to the extended crosslinking of alginate chains and hence, to a more compact network [9]. The spectra of the synthesized IPNs present characteristic bands of both pure compounds. Peak at 1612 cm^{-1} assigned to -COO⁻ group of alginate is superposed to the signals of carbonyl and amino groups of pAAm at 1670 cm^{-1} and 1622 cm^{-1} . Band of symmetrical vibration of -COO⁻ group at 1420 cm^{-1} was superposed with pAAm signals at 1454 cm^{-1} and 1419 cm^{-1} . No shift of the superposed peaks at around $1600\text{-}1350\text{ cm}^{-1}$ was observed giving evidence of the formation of two independent pAAm and alginate networks.

Structural and mechanical properties of hydrogels

In order to study the influence of cation's valency and crosslinkers concentrations on the structural properties of poly(acrylamide)/alginate IPN hydrogels, Young's modulus was evaluated. Mechanical properties of hydrogels were investigated by compressive strain-stress measurements. The series of simultaneous IPN hydrogels with various concentrations of Ca^{2+} ions and MBAA/AAm ratio were prepared (Table 1, compositions n° 17 - 37) in order to determine its influence on mechanical properties of the materials. Dependence of the Young's modulus, calculated from the compression measure is given in the Figure 1 as function of the crosslinker concentration.

Whatever the nature or concentration of the crosslinkers CaSO_4 or $\text{CaCl}_2/\text{Na}_2\text{SO}_4$ (Figure 1), elastic modulus increases until a maximum around $2.1 \times 10^{-4}\text{ mol}$, then decreases. This behavior could be explained by the rapid increase of viscosity of monomer solution that hinders dispersion and homogeneous distribution of the ions Ca^{2+} . Moreover, gelation rate of the alginate crosslinking increase with the Ca^{2+} ions concentration and temperature [18]. This effect leads to the formation of structurally inhomogeneous and turbid material with low crosslinking density (Table 3) and elastic modulus.

In the same manner as described for the Young's modulus, the apparent crosslinking density increases with the ionic concentration

Ion type	$\nu_{\text{as COO}}$	$\nu_{\text{s COO}}$	$\nu_{\text{M-O}}$
Na^+	1612	1421	822
Ca^{2+}	1631	1436	825
Fe^{2+}	1628	1441	821
Fe^{3+}	1634	1446	810

Table 2: Infrared frequencies (cm^{-1}) for metal-alginate complexes.

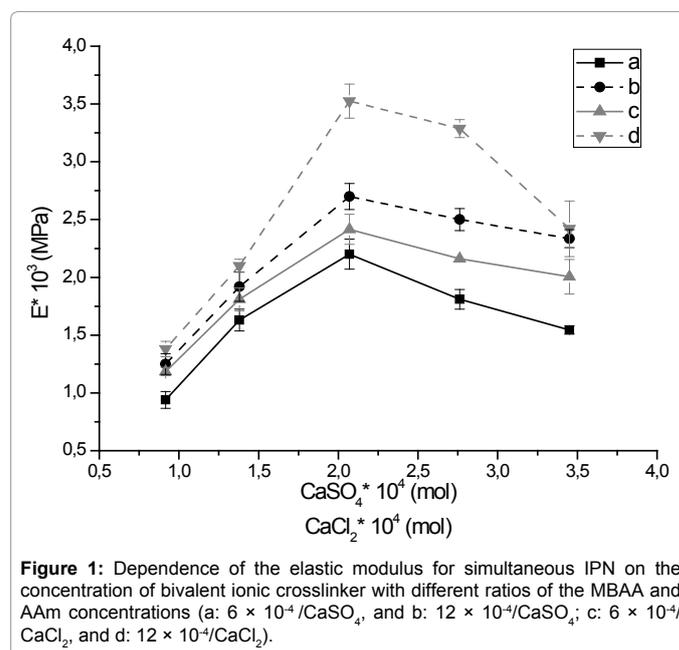


Figure 1: Dependence of the elastic modulus for simultaneous IPN on the concentration of bivalent ionic crosslinker with different ratios of the MBAA and AAm concentrations (a: $6 \times 10^{-4}/\text{CaSO}_4$, and b: $12 \times 10^{-4}/\text{CaSO}_4$; c: $6 \times 10^{-4}/\text{CaCl}_2$, and d: $12 \times 10^{-4}/\text{CaCl}_2$).

[Cations], mol.		MBAA/AAm $\times 10^4$	$n_e \times 10^6$, mol/cm ³
0.917	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	6	1.91
1.38	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	6	2.99
2.07	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	6	3.55
2.76	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	6	3.16
3.45	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	6	2.84
0.92	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	12	2.3
1.38	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	12	3.41
2.07	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	12	4.28
2.76	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	12	4.27
3.45	$\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$	12	4.12
0.92	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	6	2.4
1.38	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	6	3.32
2.07	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	6	3.90
2.76	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	6	3.77
3.45	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	6	3.69
0.92	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	12	2.53
1.38	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	12	3.73
2.07	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	12	5.59
2.76	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	12	5.61
3.45	$\text{Ca}^{2+}, \text{CaCl}_2/\text{Na}_2\text{SO}_4$	12	4.27

Table 3: Apparent cross-linking densities of the simultaneous IPN hydrogels (cation: $\text{Ca}^{2+}, \text{CaSO}_4 \times x\text{H}_2\text{O}$, 2 mol/L).

till a maximum and decreases in case of inefficient ionic crosslinking (due to rapid gelation of the alginate chains). We assume that such an instantaneous gelation of alginate creates highly crosslinked zones alginate beads in the monomer solution before the radical polymerization occurs. These highly crosslinked zones of alginate network act as obstructions for distribution of polyacrylamide network in volume leading to structurally inhomogeneous material.

In order to study the routes improving the stiffness of these hydrogels, several approaches were applied. The first one deals with the synthesis procedure since the sequential procedure allows introducing a greater amount of cations for the alginate crosslinking. The second one is focused on the influence of the ionic valence and series of IPN hydrogels were prepared with Fe^{3+} ions and compared to that formed

in the presence of Fe^{2+} ions. With the third one, the amount of the covalent crosslinker of acrylamide was increased up to 40 times (Table 1, compositions n° 1 - 16). Alginate chains were crosslinked by the swelling in saturated solutions of iron salts (2 mol/L) for 24h. Stiff hydrogels with elastic modulus up to 0.15 MPa were obtained (Figure 2).

Elastic modulus of hydrogels increases proportionally to the concentration of covalent crosslinking molecules in the composition (Figure 2), which is in accordance with the rubber elasticity theory. If comparing the pure polyacrylamide hydrogel with the semi-IPN pAAm/alginate, we may conclude that there is no influence of interpenetrating alginate chains on the elastic modulus of the system. However, comparison of pure pAAm and semi-IPN pAAm/alginate with full-IPN hydrogels shows that the elastic modulus increases significantly in case of the full-IPN systems. Such increase becomes more important for the hydrogels crosslinked by Fe^{3+} ions. This behavior can be explained by the ability of trivalent ions to bond three carboxylic group of different alginate chains resulting in a tridimensional bonding structure with coordinating number $(\text{COO})_3\text{M}$. Calculated values of apparent crosslinking density show that the trivalent bonding structure leads to more compact networks (Figure 2). Such behavior is due to crosslinking of three alginate chains at the same reticulation point. Improvement of the elastic modulus of hydrogels is possible by increase the alginate molecular weight and/or its composition (G-blocks proportion in the structure) [17]. Viscosity of the alginate solution could significantly increase with high molecular weight alginate (Cargill Algogel 6021; $M_w = 2 \times 10^5$ g/mol) resulting in difficulties to blend it with the other components and consequently to form a homogeneous material. In this work, we describe an easy route avoiding alginate solution inhomogeneity caused by high viscosity at the pre-polymerization stage using two types of alginates with different molecular weight which were mixed together and Alginate2 solution prepared (70 wt% of sodium alginate (Sigma - Aldrich) and 30 wt% of Algogel 6021 (Cargill)). However, the analysis of M-blocks to G-blocks ratio is required to make a full conclusion about the chemical structure difference between these two commercial products.

From the Figure 3 showing the elastic modulus of Alginate2 based IPN hydrogels, it appears that these hydrogels possess higher modulus than those based on the alginate (Alginate1) with lower molar mass. For the hydrogels formed in presence of the Fe^{3+} , the curve passes through

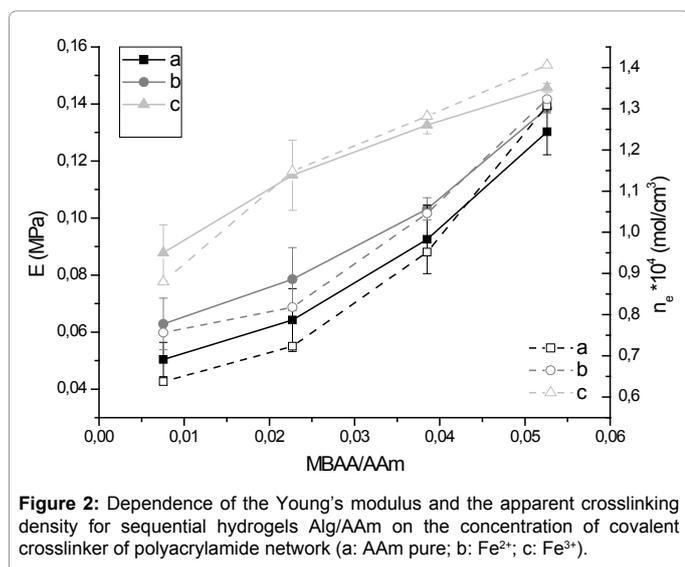


Figure 2: Dependence of the Young's modulus and the apparent crosslinking density for sequential hydrogels Alg/AAm on the concentration of covalent crosslinker of polyacrylamide network (a: AAm pure; b: Fe^{2+} ; c: Fe^{3+}).

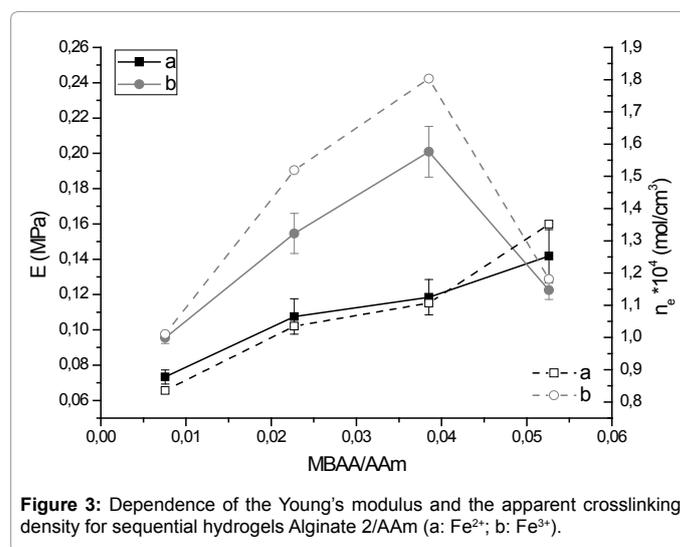


Figure 3: Dependence of the Young's modulus and the apparent crosslinking density for sequential hydrogels Alginate 2/AAm (a: Fe^{2+} ; b: Fe^{3+}).

up to maximum of 0.2 MPa at 0.04 MBAA/AAm and then sharply decreases. At this concentration, it is assumed that the covalently crosslinked polyacrylamide network possess too high density that prevent the effective crosslinking of alginate chains penetrating it. However, with the exception of the case of over-crosslinked networks represented by inflection point, hydrogels formed with Fe^{3+} ions are 30% - 100% stiffer. The results obtained for the hydrogels prepared by a two-step procedure show that this procedure combined with the use of trivalent ions and composition of the alginate with high gelation ability is an efficient way to improve the stiffness of polyacrylamide/alginate hydrogels.

Swelling properties

Swelling behavior of simultaneous and sequential hydrogels prepared using different ions ($\text{Ca}^{2+}/\text{Fe}^{2+}/\text{Fe}^{3+}$) was determined in terms of the equilibrium water content (Figures 4 and 5). The water content of the hydrogels prepared in simultaneous route in the presence of Ca^{2+} ions is higher than that of pure pAAm (90%) and lower than with pure alginate (Figure 4). However, with that latter case, the hydrogel is not formed because of the water solubility of the alginate at low crosslinking density avoiding any ionic bonds creation. In this type of preparation process, both polymeric components have a competitive and opposite effect, i.e., the dissolution of the alginate and the non-solubility of the polyacrylamide. Comparing to the apparent network density values, it appears that the water uptake strongly depends on the free volume and so, on the network mesh size. From the Figure 4, we may notice that water uptake decreases in the same manner as the network density rises.

Equilibrium water content was also estimated for IPN hydrogels made in sequential route (Figure 5). We could see that the water content decreases with the density of crosslinks as expected [21-23]. It is remarkable that the water content of hydrogels with Fe^{2+} as crosslinker are 5-7% higher than that of hydrogels with Fe^{3+} . When trivalent ions are used for crosslinking, additional bonds between chains lead to the formation of a three-dimensional structure. The obtained higher density of crosslinks compared to that in case of bivalent ions induces the decrease of the free volume and the water content. No noticeable difference in the water content between compositions with different types of the alginate in the presence of the trivalent ions was found. We consider that in the case of tridimensional bonding structure decrease

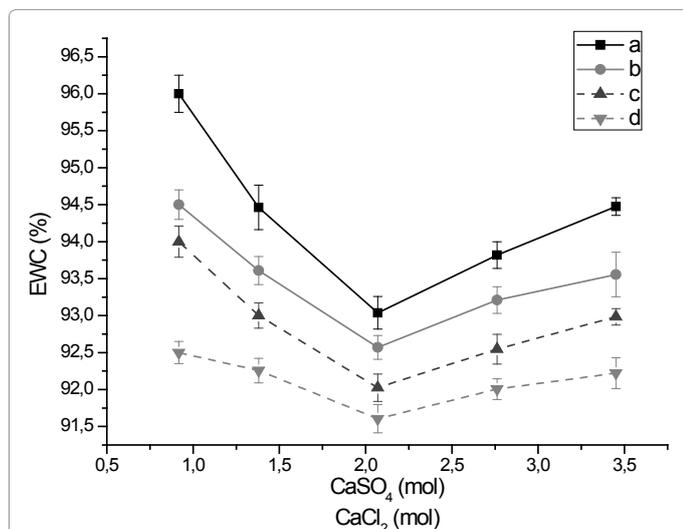


Figure 4: Dependence of equilibrium water content at 37°C for simultaneous IPNs on the concentration of bivalent ionic crosslinker with different ratio of the MBAA and AAm concentrations (a: 6×10^{-4} /CaSO₄, b: 12×10^{-4} /CaSO₄; c: 6×10^{-4} /CaCl₂, and d: 12×10^{-4} /CaCl₂).

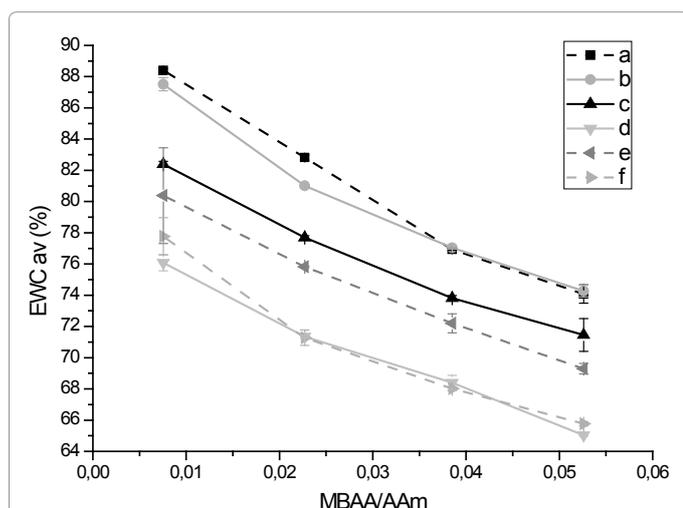


Figure 5: Dependence of equilibrium water content at 37°C for sequential hydrogels Alg/AAm on the concentration of covalent crosslinker of polyacrylamide network (a: AAm pure; b: Alg.1/AAm; c: Alg.1/AAm Fe²⁺; d: Alg.1/AAm Fe³⁺; e: Alg.2/AAm Fe²⁺; Alg.2/AAm Fe³⁺).

of free volume neglects the effect of alginate on the water content. For these hydrogels, the free volume becomes limiting factor of the water uptake and EWC decrease proportional to reduction of it. However, about a 2%-3% higher EWC was obtained for the Alginate1/Fe²⁺ hydrogels comparing to the Alginate2/Fe²⁺ indicating the effect of the alginate composition.

Conclusion

IPN hydrogels based on ionically crosslinked alginate and covalently crosslinked polyacrylamide were prepared using two different processes and various multivalent ions. Swelling and mechanical properties of the prepared hydrogels were studied depending on the ions valence and crosslinking density of each network. Several approaches were combined to obtain stiff hydrogels required for certain biomedical applications. It was shown that two-step polymerization process is

absolutely necessary to combine two highly crosslinked polymer networks. Use of trivalent ions for crosslinking of adapted alginate composition, combined with dense polyacrylamide network by two-step synthesis process allows obtaining highly stiff IPN hydrogels. On the other hand, it was not possible to prepare same hydrogels by simultaneous route because of the instantaneous character of alginate crosslinking resulting in the structurally inhomogeneous materials.

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